

(12) **United States Patent**
Curran et al.

(10) **Patent No.:** **US 9,180,021 B2**
(45) **Date of Patent:** ***Nov. 10, 2015**

(54) **SYSTEMS AND METHODS FOR SPINAL FUSION**

(71) Applicant: **NuVasive, Inc.**, San Diego, CA (US)

(72) Inventors: **Matthew Curran**, Carlsbad, CA (US);
Mark Peterson, Medford, OR (US);
Luiz Pimenta, Sao Paulo (BR)

(73) Assignee: **NuVasive, Inc.**, San Diego, CA (US)

(*) Notice: Subject to any disclaimer, the term of this patent is extended or adjusted under 35 U.S.C. 154(b) by 0 days.

This patent is subject to a terminal disclaimer.

(21) Appl. No.: **14/314,823**

(22) Filed: **Jun. 25, 2014**

(65) **Prior Publication Data**

US 2014/0309742 A1 Oct. 16, 2014

Related U.S. Application Data

(63) Continuation of application No. 14/171,484, filed on Feb. 3, 2014, now Pat. No. 8,814,940, which is a continuation of application No. 14/066,285, filed on Oct. 29, 2013, now Pat. No. 8,685,105, which is a

(Continued)

(51) **Int. Cl.**

A61F 2/44 (2006.01)

A61F 2/46 (2006.01)

(52) **U.S. Cl.**

CPC **A61F 2/4455** (2013.01); **A61F 2/442** (2013.01); **A61F 2/447** (2013.01); **A61F 2/4611** (2013.01); **A61F 2/44** (2013.01)

(58) **Field of Classification Search**

CPC **A61F 2/4455**; **A61F 2/447**; **A61F 2/4611**
USPC **623/17.11-17.16**
See application file for complete search history.

(56) **References Cited**

U.S. PATENT DOCUMENTS

3,486,505	A	12/1969	Morrison
3,518,993	A	7/1970	Blake
3,604,487	A	9/1971	Gilbert
3,745,995	A	7/1973	Kraus
3,848,601	A	11/1974	Ma et al.
3,867,728	A	2/1975	Stubstad et al.
4,026,304	A	5/1977	Levy
4,026,305	A	5/1977	Brownlee et al.
4,349,921	A	9/1982	Kuntz

(Continued)

FOREIGN PATENT DOCUMENTS

CA	2015507	1/1999
EP	369603	5/1990

(Continued)

OTHER PUBLICATIONS

Final Written Decision in *Medtronic, Inc. v. NuVasive, Inc.*, Case IPR2013-00507, dated Feb. 11, 2015, 14 pages.

(Continued)

Primary Examiner — Eduardo C Robert

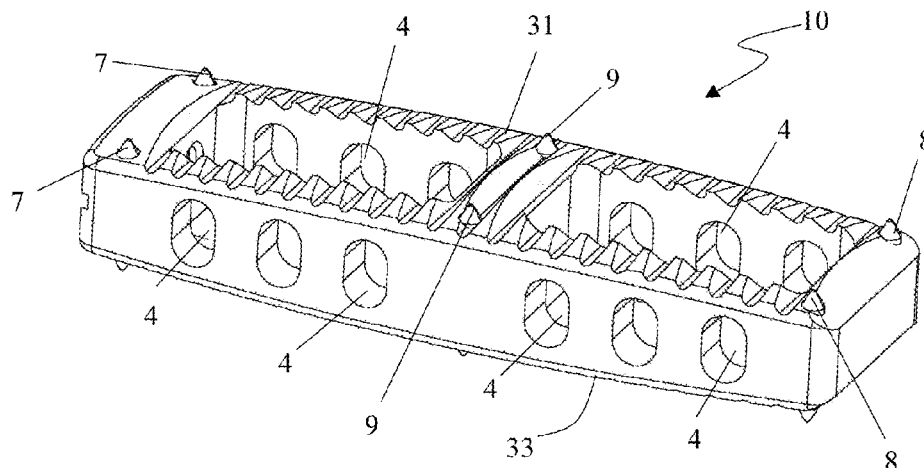
Assistant Examiner — Stuart S Bray

(74) *Attorney, Agent, or Firm* — Fish & Richardson P.C.

(57) **ABSTRACT**

A system and method for spinal fusion comprising a spinal fusion implant of non-bone construction releasably coupled to an insertion instrument dimensioned to introduce the spinal fusion implant into any of a variety of spinal target sites.

37 Claims, 20 Drawing Sheets



Related U.S. Application Data

continuation of application No. 13/748,925, filed on Jan. 24, 2013, now Pat. No. 8,574,301, which is a continuation of application No. 13/747,765, filed on Jan. 23, 2013, now Pat. No. 8,608,804, which is a continuation of application No. 13/441,092, filed on Apr. 6, 2012, now Pat. No. 8,361,156, which is a continuation of application No. 13/440,062, filed on Apr. 5, 2012, now Pat. No. 8,246,686, which is a continuation of application No. 13/079,645, filed on Apr. 4, 2011, now Pat. No. 8,187,334, which is a continuation of application No. 11/093,409, filed on Mar. 29, 2005, now Pat. No. 7,918,891.

- (60) Provisional application No. 60/557,536, filed on Mar. 29, 2004.

(56) **References Cited**

U.S. PATENT DOCUMENTS

4,454,374	A	6/1984	Pollack	5,514,180	A	5/1996	Heggeness et al.
4,501,269	A	2/1985	Bagby	5,522,879	A	6/1996	Scopelianos
4,545,374	A	10/1985	Jacobson	5,522,899	A	6/1996	Michelson
4,646,738	A	3/1987	Trott	5,524,624	A	6/1996	Tepper et al.
4,657,550	A	4/1987	Daher	5,527,312	A	6/1996	Ray
4,743,256	A	5/1988	Brantigan	5,534,030	A	7/1996	Navarro et al.
4,781,591	A	11/1988	Allen	5,540,688	A	7/1996	Navas
4,834,757	A	5/1989	Brantigan	5,545,222	A	8/1996	Bonutti
4,877,020	A	10/1989	Vich	5,545,688	A	8/1996	Huang
4,878,915	A	11/1989	Brantigan	5,562,736	A	10/1996	Ray et al.
4,932,975	A	6/1990	Main et al.	5,565,005	A	10/1996	Erickson et al.
4,950,296	A	8/1990	McIntyre	5,571,190	A	11/1996	Ulrich et al.
4,961,740	A	10/1990	Ray et al.	5,571,192	A	11/1996	Schonhoffer
4,962,766	A	10/1990	Herzon	5,593,409	A	1/1997	Michelson
5,015,247	A	5/1991	Michelson	5,607,424	A	3/1997	Tropiano
5,026,373	A	6/1991	Ray et al.	5,609,636	A	3/1997	Kohrs et al.
5,047,055	A	9/1991	Bao et al.	5,611,800	A	3/1997	Davis et al.
5,055,104	A	10/1991	Ray	5,611,810	A	3/1997	Arnold et al.
5,062,845	A	11/1991	Kuslich et al.	5,632,747	A	5/1997	Scarborough et al.
5,071,437	A	12/1991	Steffee	5,645,596	A	7/1997	Kim et al.
5,092,572	A	3/1992	Litwak et al.	5,645,598	A	7/1997	Brosnahan et al.
5,133,717	A	7/1992	Chopin	5,653,761	A	8/1997	Pisharodi
5,133,755	A	7/1992	Brekke	5,653,762	A	8/1997	Pisharodi
5,171,278	A	12/1992	Pisharodi	5,658,336	A	8/1997	Pisharodi
5,192,327	A	3/1993	Brantigan	5,658,337	A	8/1997	Kohrs et al.
5,217,497	A	6/1993	Mehdian	5,662,710	A	9/1997	Bonutti
5,263,953	A	11/1993	Bagby	5,665,122	A	9/1997	Kambin
5,269,785	A	12/1993	Bonutti	5,669,909	A	9/1997	Zdeblick et al.
5,284,153	A	2/1994	Raymond et al.	5,676,703	A	10/1997	Gelbard
5,290,494	A	3/1994	Coombes et al.	5,683,394	A	11/1997	Rinner
5,300,076	A	4/1994	Lerliche	5,683,400	A	11/1997	McGuire
5,304,210	A	4/1994	Crook	5,683,464	A	11/1997	Wagner et al.
5,306,307	A	4/1994	Senter et al.	5,690,629	A	11/1997	Asher et al.
5,306,309	A	4/1994	Wagner et al.	5,700,264	A	12/1997	Zucherman et al.
5,322,505	A	6/1994	Krause et al.	5,700,291	A	12/1997	Kuslich et al.
5,334,205	A	8/1994	Cain	5,700,292	A	12/1997	Margulies
5,336,223	A	8/1994	Rogers	5,702,449	A	12/1997	McKay
5,364,400	A	11/1994	Rego, Jr. et al.	5,702,451	A	12/1997	Biedermann et al.
5,395,372	A	3/1995	Holt et al.	5,702,453	A	12/1997	Rabbe et al.
5,397,363	A	3/1995	Gelbard	5,702,454	A	12/1997	Baumgartner
5,397,364	A	3/1995	Kozak	5,702,455	A	12/1997	Saggar
5,405,391	A	4/1995	Henderson et al.	5,703,451	A	12/1997	Yamamichi
5,413,602	A	5/1995	Metz-Stavenhagen	5,707,373	A	1/1998	Sevrain et al.
5,425,772	A	6/1995	Brantigan	5,711,957	A	1/1998	Patat et al.
5,431,658	A	7/1995	Moskovich	5,716,415	A	2/1998	Steffee
5,443,514	A	8/1995	Steffee	5,720,748	A	2/1998	Kuslich et al.
5,443,515	A	8/1995	Cohen et al.	5,720,751	A	2/1998	Jackson
5,445,639	A	8/1995	Kuslich et al.	5,728,159	A	3/1998	Stroeve et al.
5,454,811	A	10/1995	Huebner	5,741,253	A	4/1998	Michelson
5,458,638	A	10/1995	Kuslich et al.	5,741,261	A	4/1998	Moskovitz et al.
5,484,403	A	1/1996	Yoakum et al.	5,755,797	A	5/1998	Baumgartner
5,484,437	A	1/1996	Michelson	5,766,252	A	6/1998	Henry et al.
5,489,307	A	2/1996	Kuslich et al.	5,772,661	A	6/1998	Michelson
5,489,308	A	2/1996	Kuslich et al.	5,775,331	A	7/1998	Raymond et al.
				5,775,797	A	7/1998	Henstra
				5,779,642	A	7/1998	Nightengale
				5,782,830	A	7/1998	Farris
				5,782,919	A	7/1998	Zdeblick et al.
				5,785,710	A	7/1998	Michelson
				5,797,909	A	8/1998	Michelson
				5,800,549	A	9/1998	Bao et al.
				5,800,550	A	9/1998	Sertich
				5,814,084	A	9/1998	Grivas et al.
				5,814,550	A	9/1998	Wolcott
				5,851,084	A	12/1998	Nishikawa
				5,851,208	A	12/1998	Trott
				5,860,973	A *	1/1999	Michelson 606/247
				5,865,845	A	2/1999	Thalgott
				5,865,848	A	2/1999	Baker
				5,885,299	A	3/1999	Winslow et al.
				5,888,219	A	3/1999	Bonutti
				5,888,224	A	3/1999	Beckers et al.
				5,893,890	A	4/1999	Pisharodi
				5,904,719	A	5/1999	Errico et al.
				5,910,315	A	6/1999	Stevenson et al.
				5,942,698	A	8/1999	Stevens
				5,954,769	A	9/1999	Rosenlicht
				5,968,098	A	10/1999	Winslow
				5,993,474	A	11/1999	Ouchi

(56)

References Cited

U.S. PATENT DOCUMENTS

6,003,426	A	12/1999	Kobayashi et al.	6,989,031	B2 *	1/2006	Michelson	623/17.11
6,004,326	A	12/1999	Castro et al.	7,018,416	B2 *	3/2006	Hanson et al.	623/17.16
6,008,433	A	12/1999	Stone	D530,423	S *	10/2006	Miles et al.	D24/155
6,015,436	A	1/2000	Schonhuffer	7,125,425	B2	10/2006	Foley et al.	
6,033,405	A	3/2000	Winslow et al.	7,192,447	B2	3/2007	Rhoda	
6,033,438	A	3/2000	Bianchi et al.	7,244,258	B2	7/2007	Burkus et al.	
6,039,761	A	3/2000	Li et al.	7,303,583	B1	12/2007	Schaer et al.	
6,042,582	A	3/2000	Ray	7,326,251	B2	2/2008	McCombe et al.	
6,045,580	A	4/2000	Scarborough et al.	7,867,277	B1	1/2011	Tohmeh	
6,045,582	A	4/2000	Prybyla	7,951,203	B2	5/2011	McCombe et al.	
6,048,342	A	4/2000	Zucherman et al.	8,021,430	B2 *	9/2011	Michelson	623/17.16
6,059,829	A	5/2000	Schlapfer et al.	8,187,334	B2	5/2012	Curran et al.	
6,063,088	A	5/2000	Winslow	8,246,686	B1 *	8/2012	Curran et al.	623/17.16
6,080,155	A	6/2000	Michelson	8,251,997	B2 *	8/2012	Michelson	606/53
6,083,225	A	7/2000	Winslow et al.	8,361,156	B2	1/2013	Curran et al.	
6,096,080	A	8/2000	Nicholson et al.	8,425,612	B2 *	4/2013	Perez-Cruet et al.	623/17.16
6,102,948	A	8/2000	Brosnahan, III	8,506,630	B2 *	8/2013	Wardlaw	623/17.11
6,120,503	A	9/2000	Michelson	8,506,636	B2	8/2013	Dye	
6,120,506	A	9/2000	Kohrs et al.	8,574,301	B2	11/2013	Curran et al.	
6,132,472	A	10/2000	Bonutti	8,579,909	B2	11/2013	Burkus et al.	
6,143,033	A	11/2000	Paul et al.	8,591,589	B2	11/2013	McCombe et al.	
6,159,211	A	12/2000	Boriani et al.	8,608,804	B2	12/2013	Curran et al.	
6,159,215	A	12/2000	Urbahns et al.	2001/0016741	A1	8/2001	Burkus et al.	
6,193,756	B1	2/2001	Studer et al.	2002/0019637	A1	2/2002	Frey et al.	
6,200,347	B1	3/2001	Anderson	2002/0058950	A1	5/2002	Winterbottom et al.	
6,224,607	B1	5/2001	Michelson	2002/0068936	A1	6/2002	Burkus et al.	
6,224,631	B1	5/2001	Kohrs	2002/0116008	A1	8/2002	Lin et al.	
6,241,769	B1	6/2001	Nicholson et al.	2002/0165550	A1	11/2002	Frey et al.	
6,241,770	B1	6/2001	Michelson	2003/0023306	A1	1/2003	Liu et al.	
6,241,771	B1	6/2001	Gresser et al.	2003/0028249	A1	2/2003	Baccelli et al.	
6,251,140	B1	6/2001	Marino et al.	2003/0100950	A1	5/2003	Moret	
6,258,125	B1	7/2001	Paul et al.	2003/0105528	A1	6/2003	Shimp et al.	
6,277,149	B1	8/2001	Boyle et al.	2003/0109928	A1	6/2003	Pasquet et al.	
6,304,487	B1	10/2001	Pawletko et al.	2003/0139812	A1	7/2003	Garcia et al.	
6,319,257	B1	11/2001	Carignan et al.	2003/0139813	A1	7/2003	Messerli	
6,371,989	B1	4/2002	Chauvin et al.	2003/0149438	A1	8/2003	Nichols et al.	
6,383,221	B1	5/2002	Scarborough et al.	2004/0024408	A1	2/2004	Burkus et al.	
6,409,766	B1	6/2002	Brett	2004/0153155	A1	8/2004	Chung et al.	
6,425,772	B1	7/2002	Bernier et al.	2004/0176775	A1	9/2004	Burkus et al.	
6,426,772	B1	7/2002	Yoneyama et al.	2004/0199251	A1	10/2004	McCombe et al.	
6,432,140	B1	8/2002	Lin	2005/0059971	A1	3/2005	Michelson	
6,440,142	B1	8/2002	Ralph et al.	2005/0187625	A1	8/2005	Wolek et al.	
6,442,814	B1	9/2002	Landry et al.	2005/0197702	A1	9/2005	Coppes et al.	
6,447,547	B1	9/2002	Michelson	2005/0203538	A1	9/2005	Lo et al.	
6,454,806	B1	9/2002	Cohen et al.	2006/0074488	A1	4/2006	Abdou	
6,468,311	B2	10/2002	Boyd et al.	2006/0142864	A1	6/2006	Cauthen	
6,491,724	B1	12/2002	Ferree	2007/0179612	A1	8/2007	Johnson et al.	
6,527,773	B1	3/2003	Lin et al.	2007/0191945	A1	8/2007	Yu et al.	
D472,634	S	4/2003	Anderson	2007/0276499	A1	11/2007	Paul et al.	
D473,650	S	4/2003	Anderson	2007/0288007	A1	12/2007	Burkus et al.	
6,547,823	B2	4/2003	Scarborough et al.	2008/0015701	A1	1/2008	Garcia et al.	
6,562,072	B1	5/2003	Fuss et al.	2008/0058838	A1	3/2008	Steinberg	
6,595,998	B2	7/2003	Johnson et al.	2008/0065219	A1	3/2008	Dye	
6,599,294	B2	7/2003	Fuss et al.	2008/0119937	A1	5/2008	McCombe et al.	
6,626,905	B1	9/2003	Schmiel et al.	2009/0222099	A1	9/2009	Liu et al.	
6,635,086	B2	10/2003	Lin	2010/0106250	A1	4/2010	Abdou	
6,648,895	B2	11/2003	Burkus et al.	2011/0112642	A1	5/2011	Tohmeh	
6,672,019	B1	1/2004	Wenz	2011/0196496	A1	8/2011	McCombe et al.	
6,676,703	B2	1/2004	Biscup	2012/0078374	A1	3/2012	Villiers et al.	
6,706,067	B2	3/2004	Shimp et al.	2012/0158141	A1	6/2012	Johnson et al.	
6,723,097	B2	4/2004	Fraser et al.	2012/0179261	A1	7/2012	Soo	
6,743,255	B2	6/2004	Ferree	2012/0209388	A1	8/2012	Curran et al.	
6,746,484	B1	6/2004	Liu et al.	2012/0215317	A1	8/2012	Curran et al.	
6,755,841	B2	6/2004	Fraser et al.	2013/0006363	A1	1/2013	Ullrich et al.	
6,761,739	B2	7/2004	Shepard	2013/0138216	A1	5/2013	Curran et al.	
6,824,564	B2	11/2004	Crozet	2013/0144390	A1	6/2013	Curran et al.	
6,830,570	B1	12/2004	Frey et al.	2013/0245771	A1	9/2013	Michelson	
D503,801	S	4/2005	Jackson					
6,923,814	B1	8/2005	Hildebrand et al.	EP	517030	5/1992		
6,942,698	B1	9/2005	Jackson	EP	667127	8/1995		
6,964,687	B1	11/2005	Bernard et al.	EP	706876	4/1996		
6,974,480	B2	12/2005	Messerli et al.	EP	716840	6/1996		
6,979,353	B2 *	12/2005	Bresina	EP	737448	10/1996		
6,984,245	B2 *	1/2006	McGahan et al.	EP	796593	9/1997		
6,986,788	B2 *	1/2006	Paul et al.	EP	880938	2/1998		
				EP	809974	4/1998		
				EP	809975	4/1998		

FOREIGN PATENT DOCUMENTS

(56)

References Cited

FOREIGN PATENT DOCUMENTS

EP	811356	4/1998
WO	90/00037	1/1990
WO	91/06261	5/1991
WO	92/14423	9/1992
WO	93/01771	2/1993
WO	94/04100	3/1994
WO	94/10928	5/1994
WO	95/01810	1/1995
WO	95/08306	3/1995
WO	96/08205	3/1996
WO	96/17564	3/1996
WO	96/41582	12/1996
WO	97/20513	6/1997
WO	97/33525	9/1997
WO	97/37620	10/1997
WO	98/09586	3/1998
WO	98/14142	4/1998
WO	98/17208	4/1998
WO	98/25539	6/1998
WO	99/08627	2/1999
WO	99/38461	8/1999
WO	00/44288	8/2000
WO	00/45712	8/2000
WO	00/45713	8/2000
WO	01/41681	6/2001
WO	01/49333	7/2001

OTHER PUBLICATIONS

Final Written Decision in *Medtronic, Inc. v. NuVasive, Inc.*, Case IPR2013-00508, dated Feb. 11, 2015, 19 pages.

Alleyne, Cargill, H., et al., "Current and future approaches to lumbar disc surgery: A literature review", *Medscape Orthopedics & Sports Medicine*, 1, [www.medscape.com/Medscape/OrthoSportsMed/1997/v01.n11/. . . /mos3057], (1997).

Baulot, et al., "Complementary anterior spondylodesis by thoracoscopy. Technical note regarding an observation", *Lyon Surg.*, 90(5):347-351 (1994).

Benini, et al., "Undercutting decompression and posterior fusion with translaminar facet screw fixation in degenerative lumbar spinal stenosis: Technique and results", *Neuro-Orthopedics*, 17/18, 159-172 (1995).

Berry, et al., "A morphometric study of human lumbar and selected thoracic vertebrae, study of selected vertebrae" *Spine* 12(4):362-367 (1996).

CoRoent® XL & XLR Marketing Brochure (9004225 B.0), *NuVasive, Inc.*, 2006, 2 pages.

CoRoent® XL & XLR Marketing Brochure (9004225 C.0), *NuVasive, Inc.*, 2007, 2 pages.

CoRoent® XL Marketing Brochure (9500039 A.0), *NuVasive, Inc.*, 2006, 8 pages.

CoRoent™ Marketing Brochure (9004001 A.0), *NuVasive, Inc.*, 2004, 2 pages.

CoRoent™ Marketing Brochure (9004001 C.0), *NuVasive, Inc.*, 2005, 2 pages.

CoRoent™ XL & XLR Marketing Brochure (9004225 A.0), *NuVasive, Inc.*, 2005, 2 pages.

Counterclaim Defendants' Corrected Amended Invalidity Contentions re U.S. Pat. Nos. 8,000,782; 8,005,535; 8,016,767; 8,192,356; 8,187,334; 8,361,156; D652,922; D666,294 re Case No. 3:12-cv-02738-CAB(MDD), dated Aug. 19, 2013, 30 pages.

Crock, H. V., "A Short Practice of Spinal Surgery", Second, revised edition, published by Springer-Verlag/Wein, New York (1993).

Crock, H. V., "Anterior Lumbar Interbody Fusion" *Clinical Orthopaedics & Related Research*, Marshall R. Urist, Editor-in-Chief, J. B. Lippincott Company (1982).

Declaration of Mary Phelps Regarding Telamon Verte-Stack PEEK Vertebral Body Spacer, dated Aug. 13, 2013, 9 pages.

Declaration of Richard A. Hynes, M.D. Regarding U.S. Pat. No. 8,187,334, dated Aug. 14, 2013, 74 pages.

Declaration of Richard A. Hynes, M.D. Regarding U.S. Pat. No. 8,361,156, dated Aug. 14, 2013, 74 pages.

Declaration of Steven D. DeRidder regarding U.S. Pat. No. 2002/0165550, Jul. 30, 2013, 5 pages.

Edeland, H.G., "Some additional suggestions for an intervertebral disc prosthesis", *Journal of Biomedical Engineering*, 7:57-62 (1985).

Kambin, et al., "History and current status of percutaneous arthroscopic disc surgery", *Spine*, 21(24S):57S-61S (1996).

Kemp, H. B. S., "Anterior fusion of the spine for infective lesions in adults", *Journal of Bone & Joint Surgery*, 55B(4):715-734 (1973).

Medtronic Sofamor Danek USA, Inc. "Boomerang I Verte-Stack PEEK Vertebral Body Brochure," 2003, 6 pages.

Medtronic Sofamor Danek USA, Inc. "Boomerang I Verte-Stack PEEK Vertebral Body Spacer Implant," Apr. 26, 2001, 8 pages.

Medtronic Sofamor Danek USA, Inc. "Boomerang II Verte-Stack PEEK Vertebral Body Spacer Brochure," 2004, 4 pages.

Medtronic Sofamor Danek USA, Inc. "Boomerang II Verte-Stack PEEK Vertebral Body Spacer Implant," Dec. 17, 2003, 9 pages.

Medtronic Sofamor Danek USA, Inc. "Boomerang Prototype Verte-Stack PEEK Vertebral Body Spacer Implant," May 7, 2000, 8 pages.

Medtronic Sofamor Danek USA, Inc. "PCR PEEK Cement Restrictor Brochure," 2001, 2 pages.

Medtronic Sofamor Danek USA, Inc. "PCR PEEK Cement Restrictor Implant," Oct. 2, 2001, 17 pages.

Medtronic Sofamor Danek USA, Inc. "Telamon Verte-Stack PEEK Vertebral Body Spacer Brochure I," 2003, 2 pages.

Medtronic Sofamor Danek USA, Inc. "Telamon Verte-Stack PEEK Vertebral Body Spacer Brochure II," 2003, 10 pages.

Medtronic Sofamor Danek USA, Inc. "Telamon Verte-Stack PEEK Vertebral Body Spacer Implant," Oct. 2, 2001, 6 pages.

NuVasive, Inc., Corrected Final Invalidity Contentions Regarding U.S. Pat. No. 5,860,973, U.S. Pat. No. 6,592,586 and U.S. Pat. No. 6,945,933 filed in the United States District Court, Southern District of California on Jun. 14, 2010 (and 23 appendices).

Petition for Inter Partes Review of U.S. Pat. No. 8,187,334 Pursuant to 35 U.S.C. 311-319, 37 C.F.R. 42, dated Aug. 14, 2013, 64 pages.

Petition for Inter Partes Review of U.S. Pat. No. 8,361,156 Pursuant to 35 U.S.C. 311-319, 37 C.F.R. 42, dated Aug. 14, 2013, 64 pages.

Second Petition for Inter Partes Review of U.S. Pat. No. 8,187,334 Pursuant to 35 U.S.C. 311-319, 37 C.F.R. 42, dated Aug. 14, 2013, 64 pages.

Second Petition for Inter Partes Review of U.S. Pat. No. 8,361,156 Pursuant to 35 U.S.C. 311-319, 37 C.F.R. 42, dated Aug. 14, 2013, 64 pages.

Stein, et al., "Percutaneous facet joint fusion: Preliminary experience", *Journal of Vascular and Interventional Radiology*, 4:69-74 (1993).

Synthes Vertebral Spacer-PR Brochure, *Synthes Spine*, 2002, 2 pages.

Synthesis Spine Vertebral Spacer-PR Implant, Jun. 2002, 2 pages.

Synthesis Spine Vertebral Spacer-TR Implant, Aug. 2002, 2 pages.

Telamon Implantation Guide, *Medtronic Sofamor Danek*, 2003, 10 pages.

Telamon Verte-Stack PEEK Vertebral Body Spacer Brochure, *Medtronic Sofamor Danek*, 2003, 2 pages.

Vamvanij, et al., "Surgical treatment of internal disc disruption: An outcome study of four fusion techniques", *Journal of Spinal Disorders*, 11(5):375-382 (1998).

Zhou et al., Geometrical dimensions of the lower lumbar vertebrae: analysis of data from digitised CT images, *Eur Spine J*, 2000, 9: 242-248.

Patent Owner NuVasive Inc.'s Preliminary Response in IPR2013-00504, dated Nov. 25, 2013, 40 pages.

Decision denying Institution of *Inter Partes* review in IPR2013-00504, dated Feb. 13, 2014, 9 pages.

Patent Owner NuVasive Inc.'s Preliminary Response in IPR2013-00506, dated Nov. 25, 2013, 38 pages.

Decision denying Institution of *Inter Partes* review in IPR2013-00506, dated Feb. 13, 2014, 21 pages.

NuVasive Inc.'s Patent Owner Response in IPR2013-00506, dated May 21, 2014, 66 pages.

Declaration of Dr. Hansen A. Yuan from IPR2013-00506, dated May 21, 2014, 63 pages.

(56)

References Cited

OTHER PUBLICATIONS

Synthes SVS-PR Guide, *Synthes Spine*, 2002, 8 pages.
 Medtronic Sofamor Danek Boomerang brochure, *Medtronic Sofamor Danek*, 2003, 6 pages.
 Synthes Vertebral Spacer—AR brochure, *Synthesis Spine*, 2006, 4 pages.
 Saber Surgical Technique/Product Catalogue, *DePuy Spine*, 2004, 12 pages.
 Petition for Inter Partes Review of U.S. Pat. No. 8,361,156 Pursuant to 35 U.S.C. 311-319, 37 C.F.R. 42, dated Mar. 5, 2014, 64 pages.
 Patent Owner NuVasive Inc.'s Preliminary Response in IPR2013-00507, dated Nov. 25, 2013, 29 pages.
 Decision denying Institution of *Inter Partes* review in IPR2013-

00507, dated Feb. 13, 2014, 15 pages.
 NuVasive Inc.'s Patent Owner Response in IPR2013-00507, dated May 21, 2014, 50 pages.
 Declaration of Dr. Hansen A. Yuan from IPR2013-00507, dated May 21, 2014, 85 pages.
 Patent Owner NuVasive Inc.'s Preliminary Response in IPR2013-00508, dated Nov. 25, 2013, 38 pages.
 Decision denying Institution of *Inter Partes* review in IPR2013-00508, dated Feb. 13, 2014, 14 pages.
 NuVasive Inc.'s Patent Owner Response in IPR2013-00508, dated May 21, 2014, 66 pages.
 Declaration of Dr. Hansen A. Yuan from IPR2013-00508, dated May 21, 2014, 85 pages.

* cited by examiner

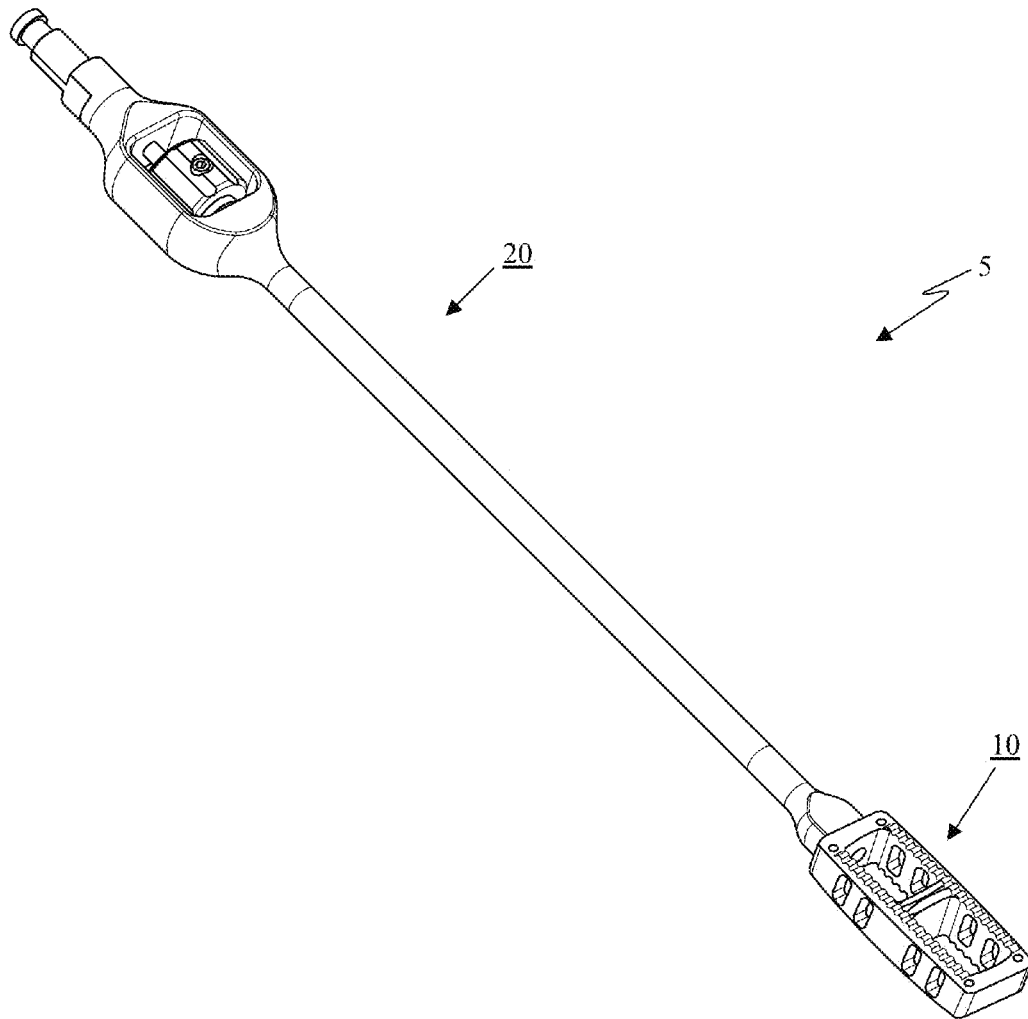
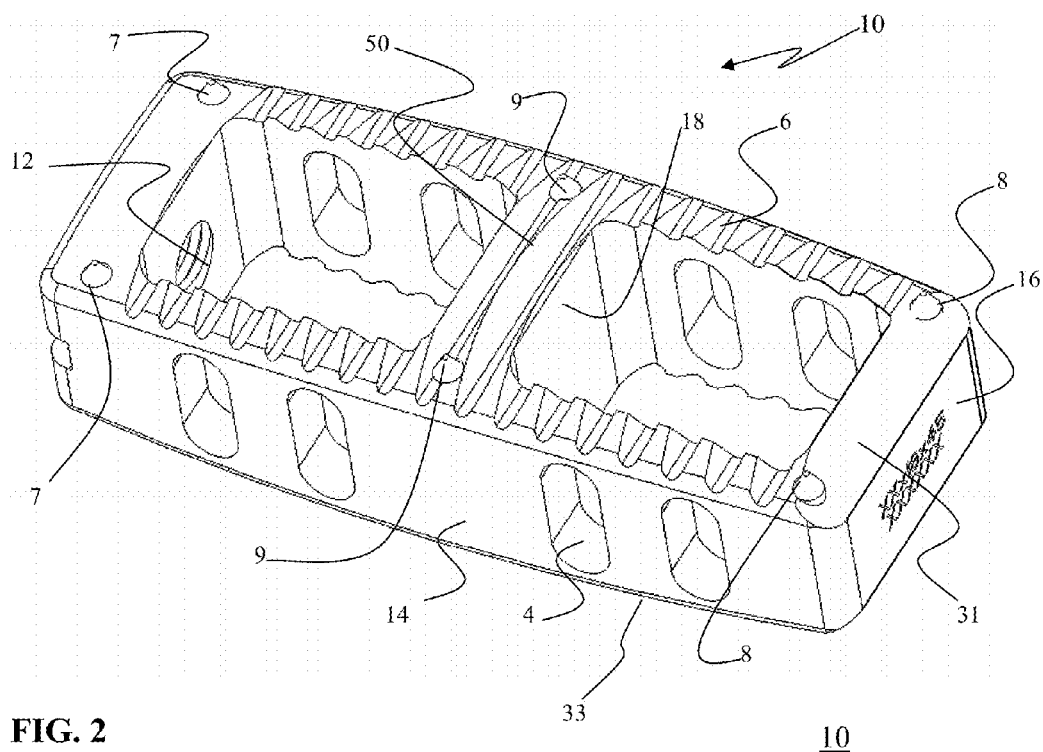


FIG. 1



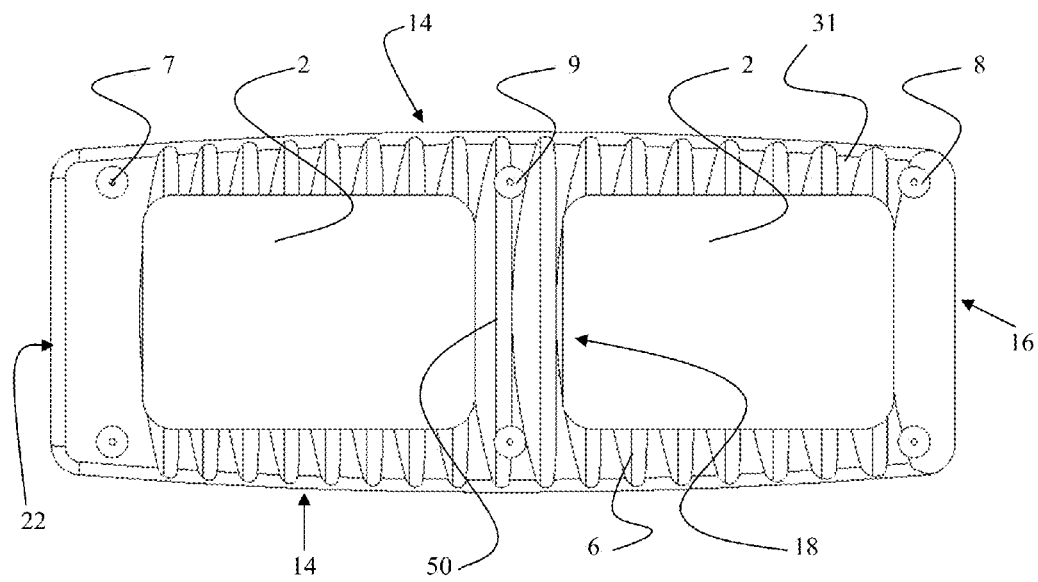


FIG. 3

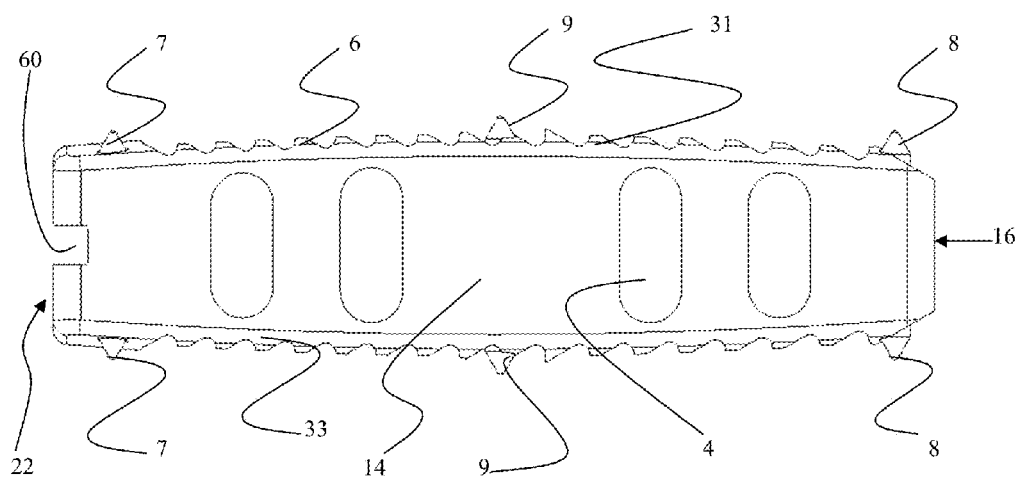


FIG. 4

10

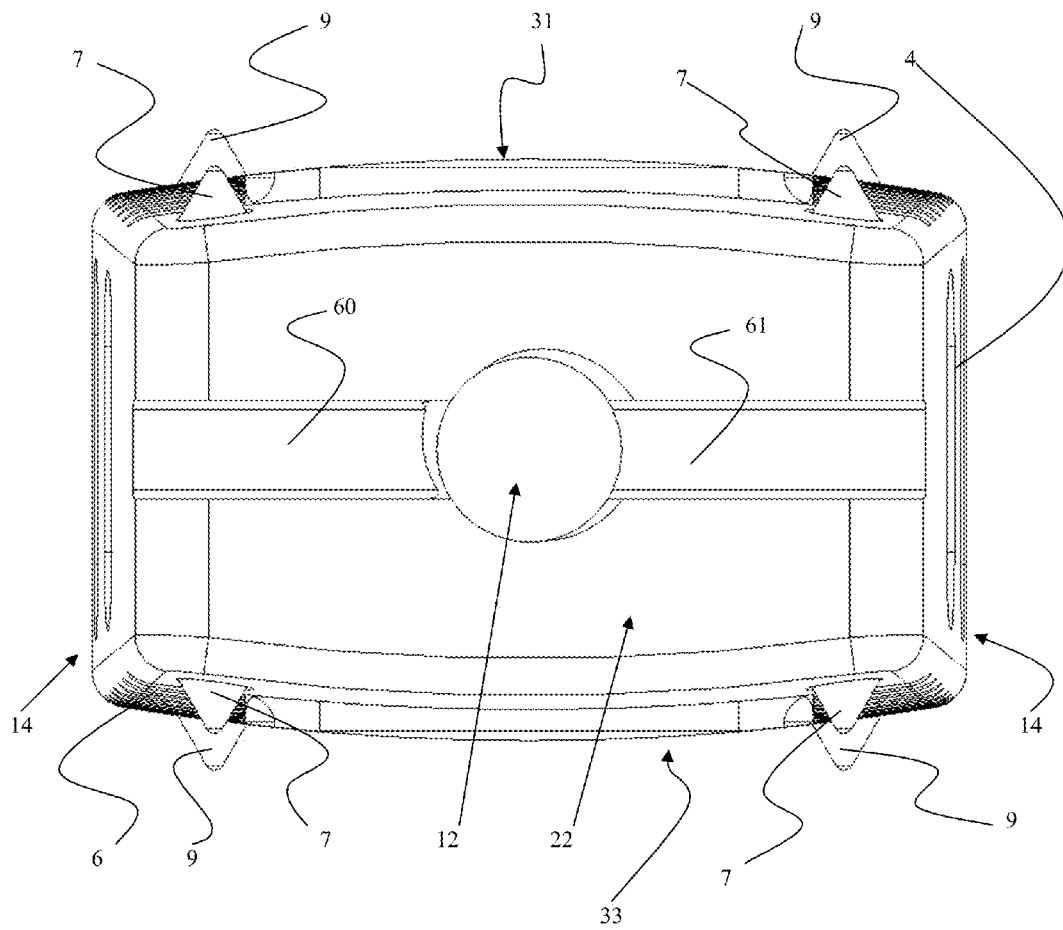


FIG. 5

10

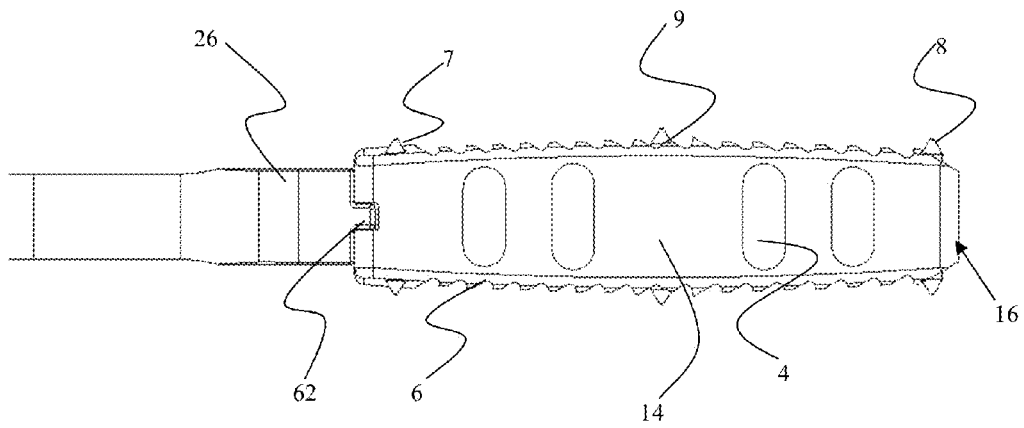


FIG. 6

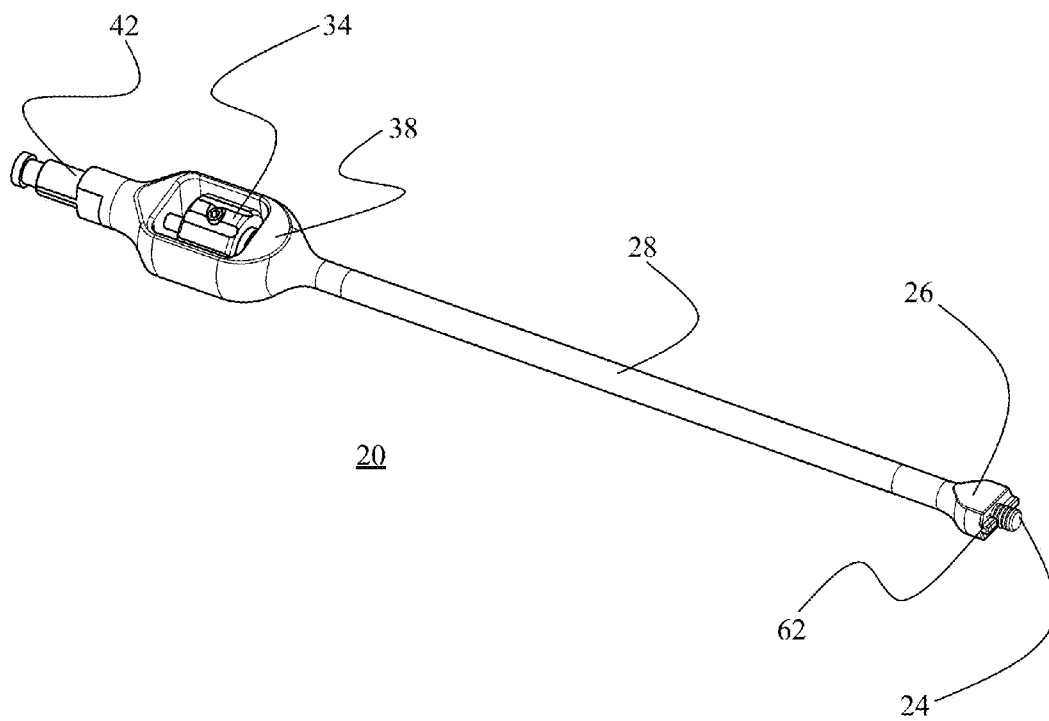
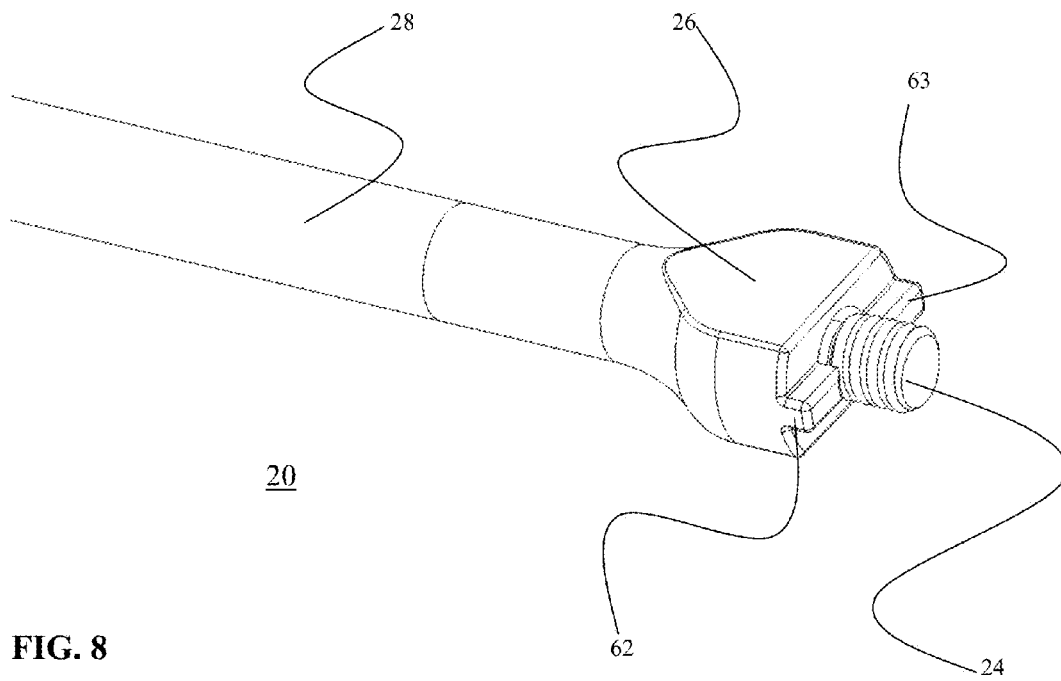


FIG. 7



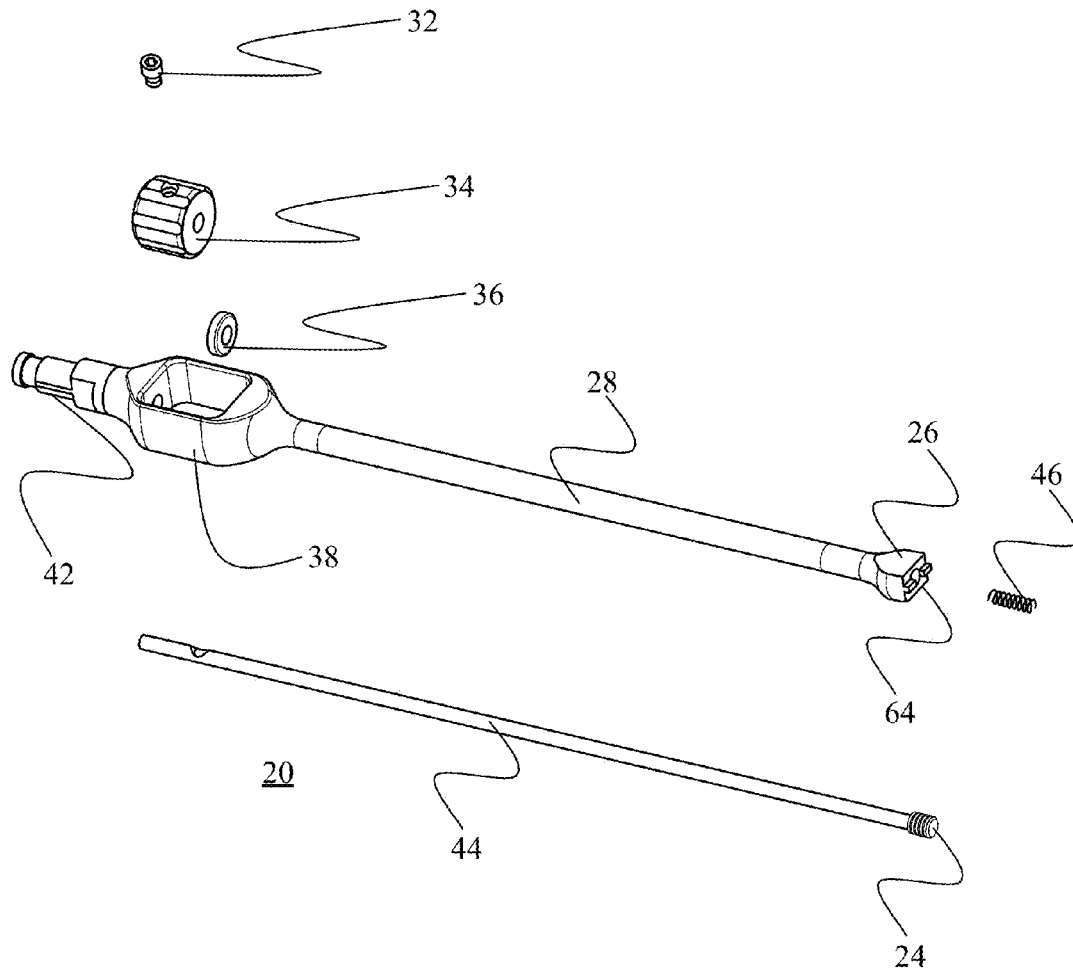


FIG. 9

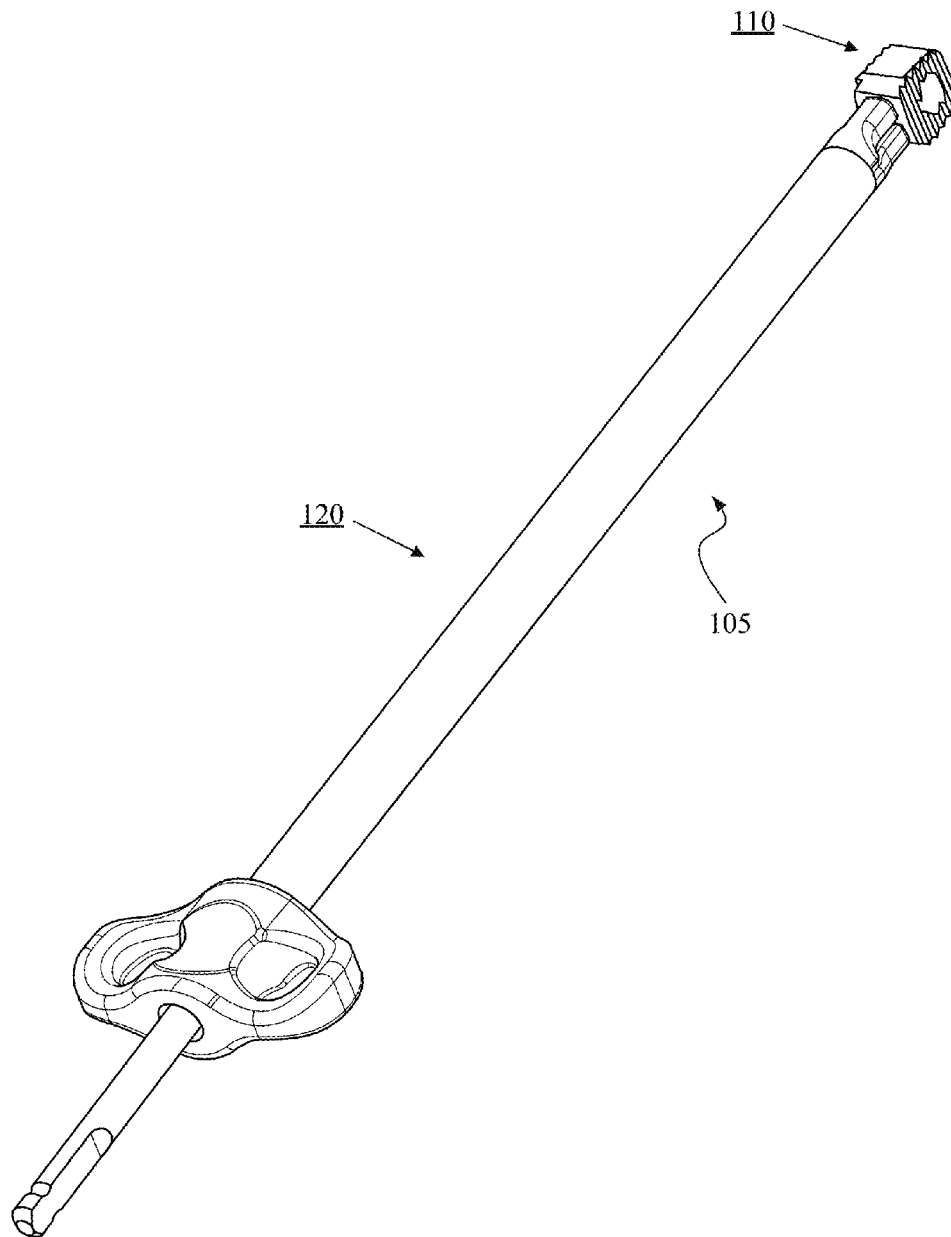
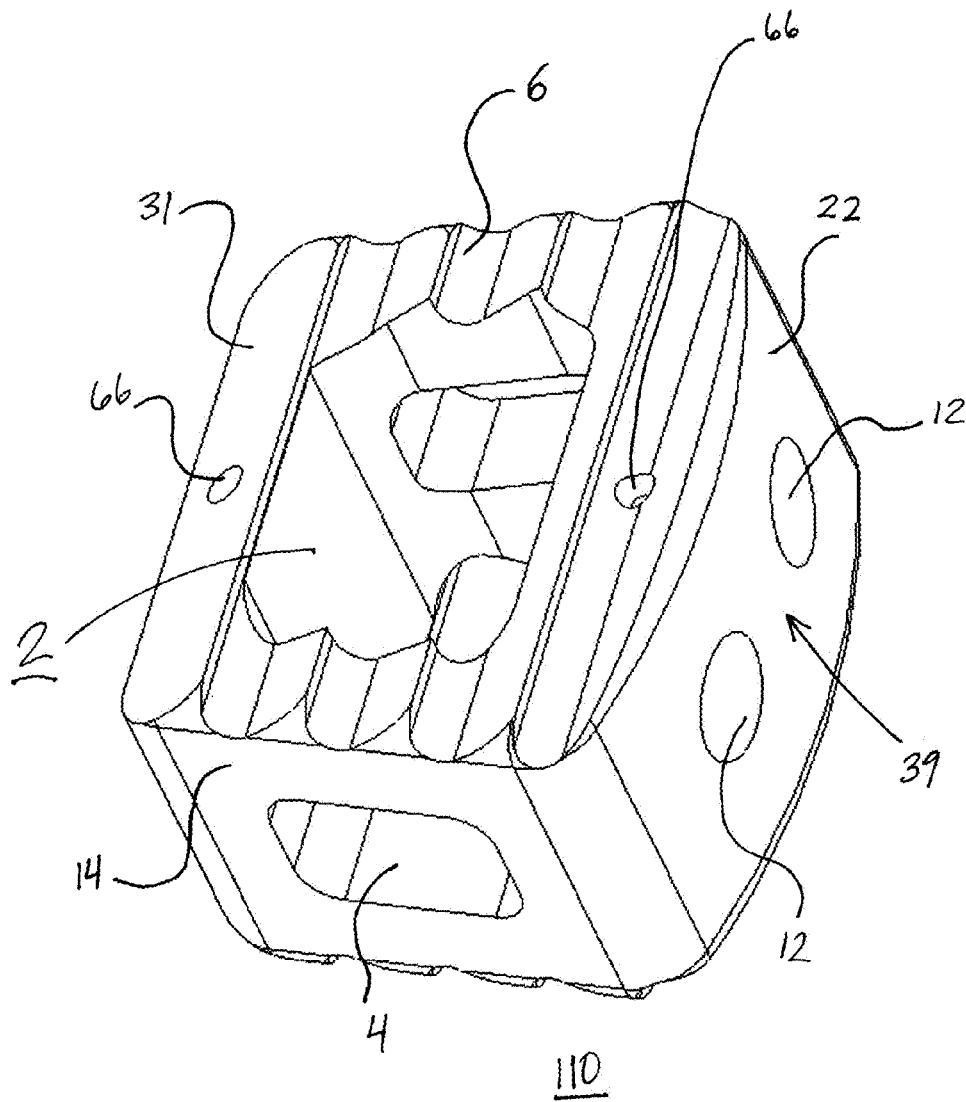
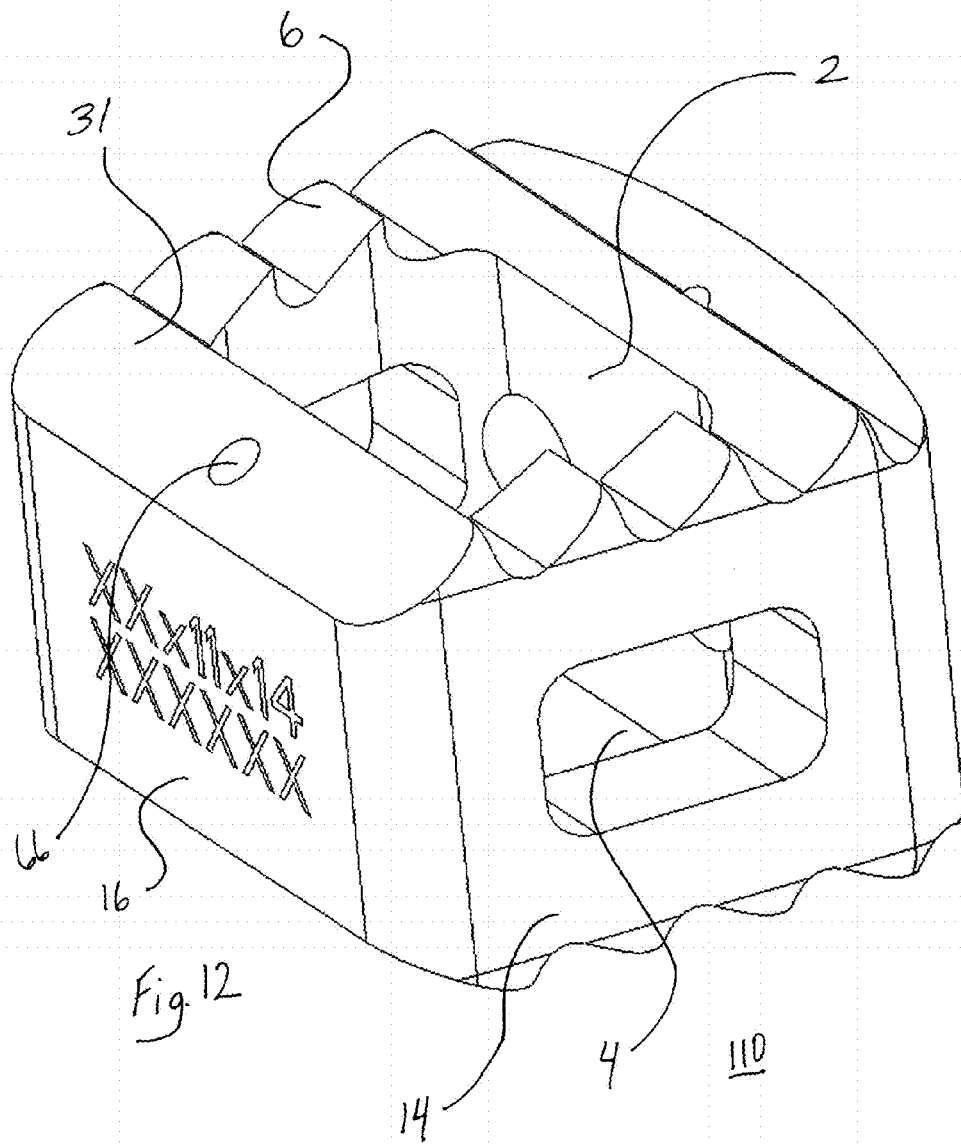
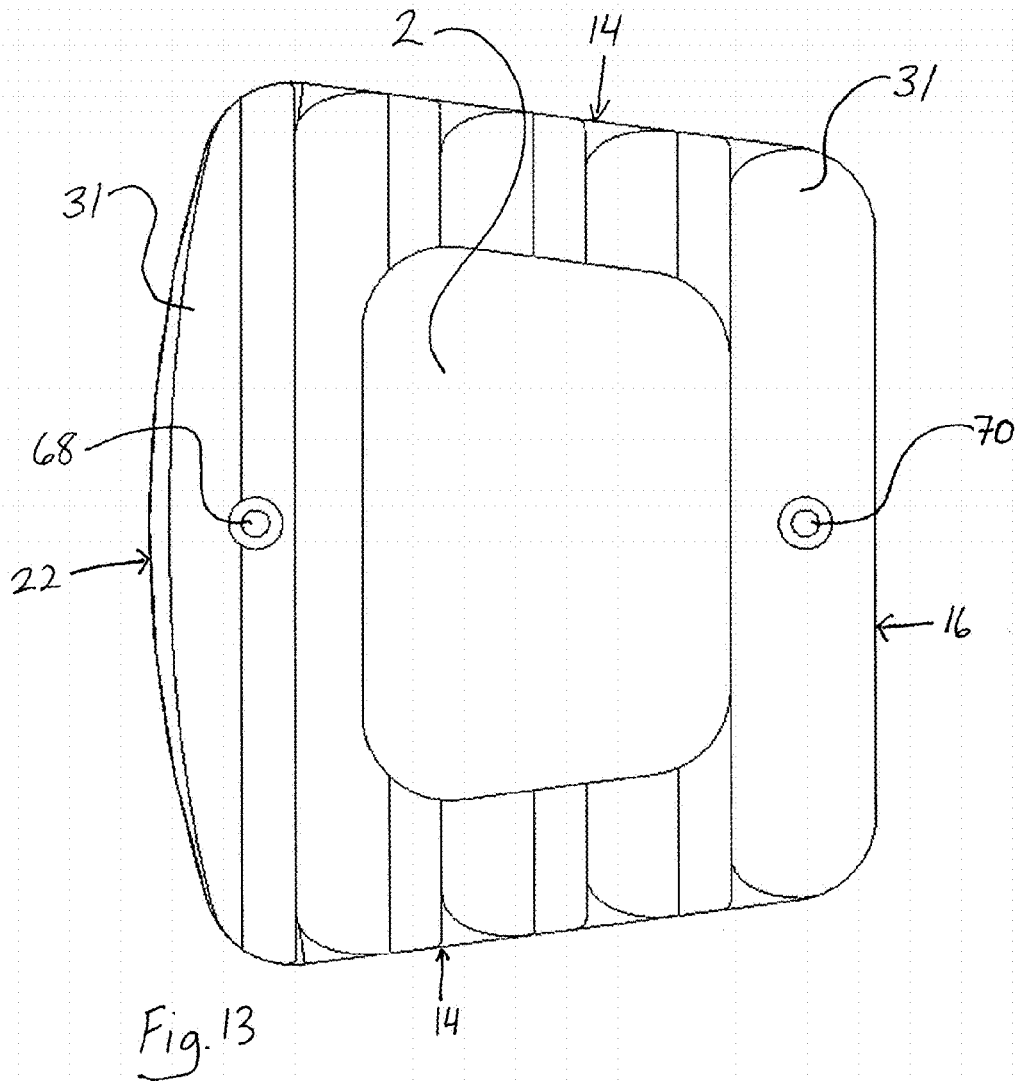
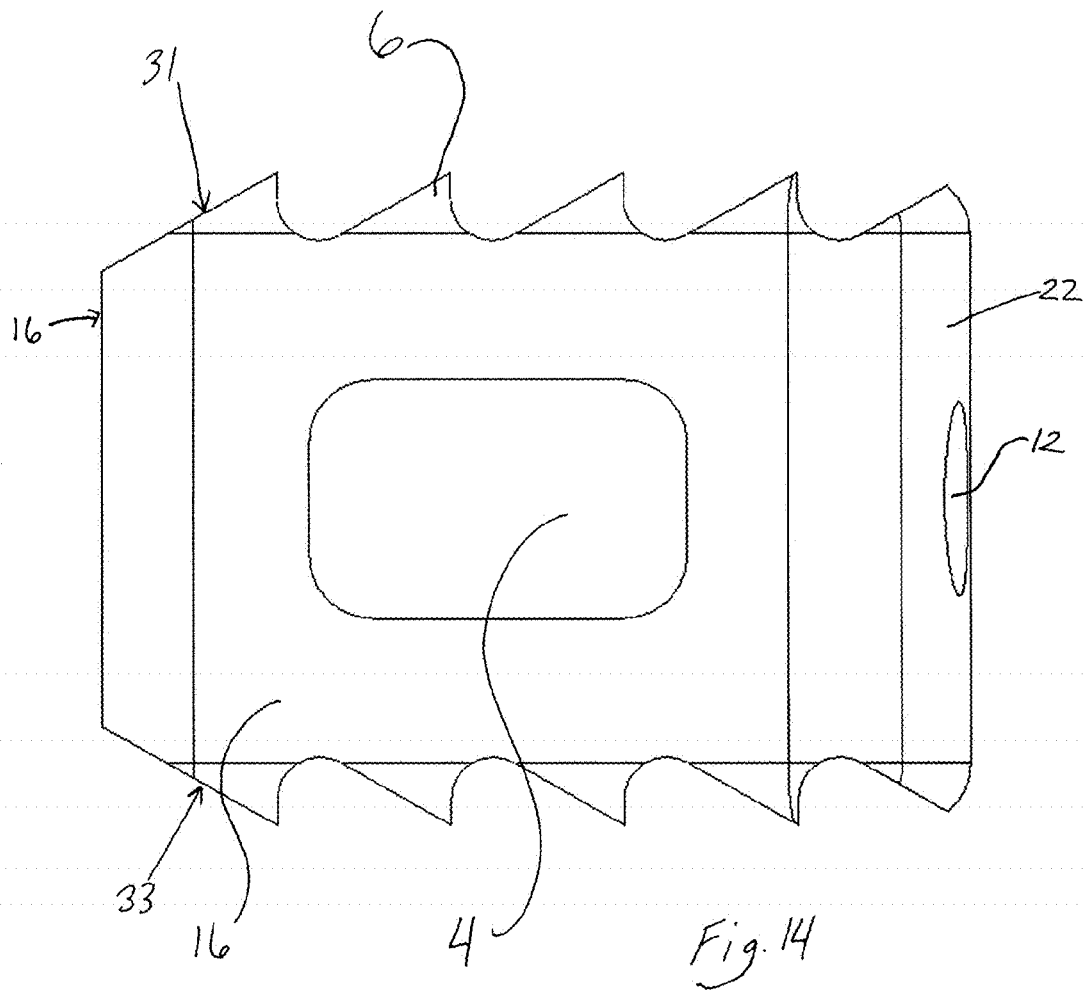


FIG. 10









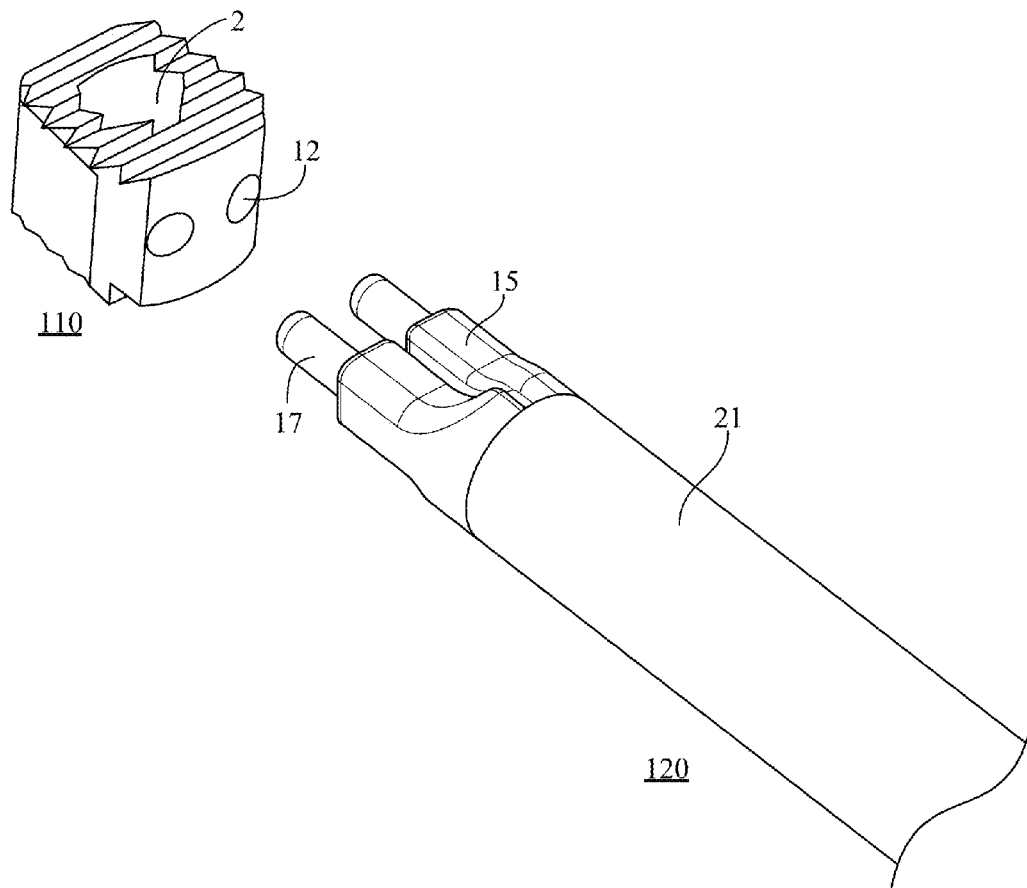


FIG. 15

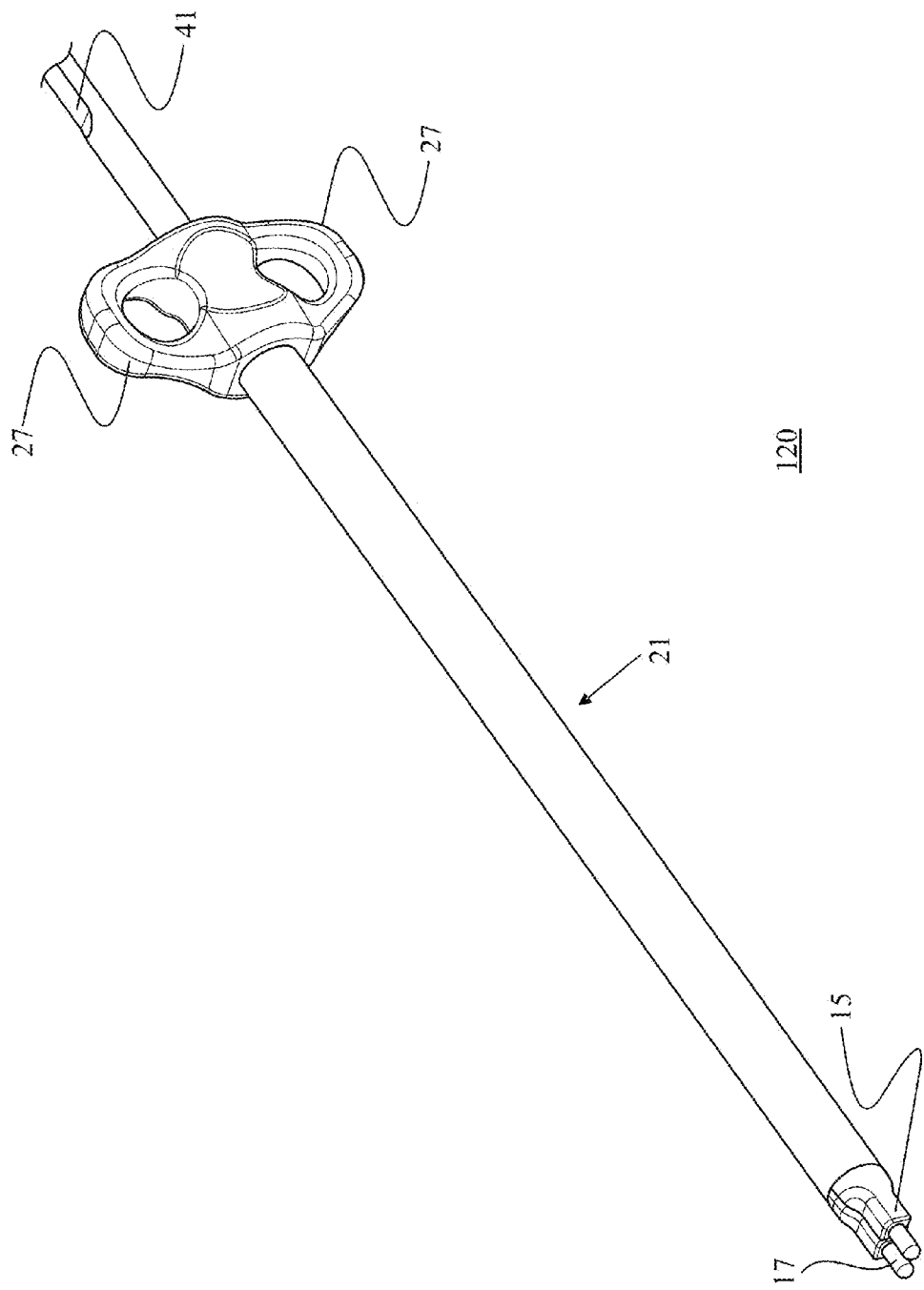


FIG. 16

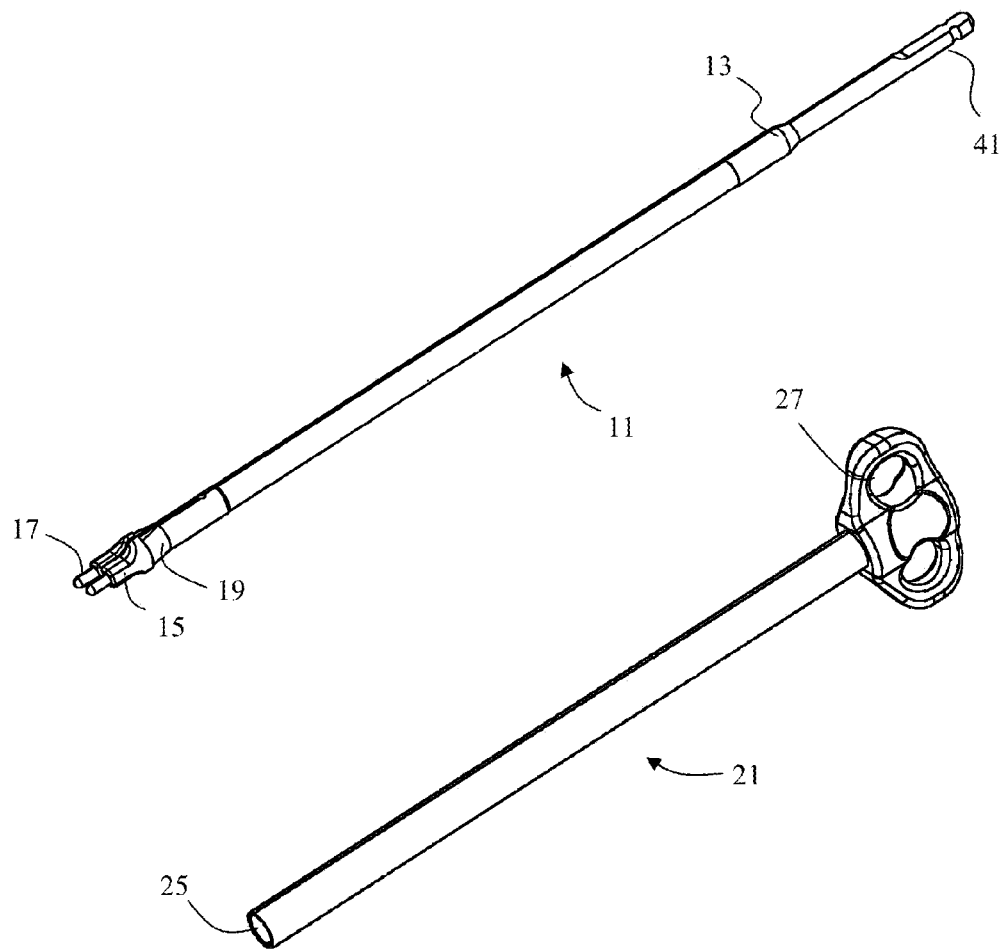


FIG. 17

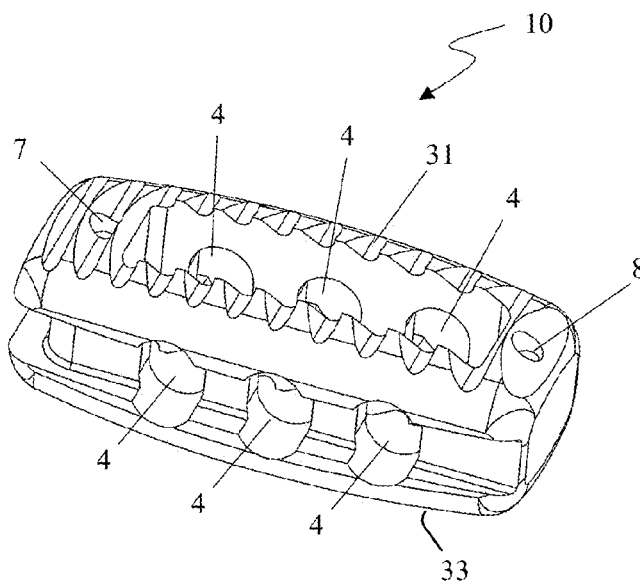


FIG. 18

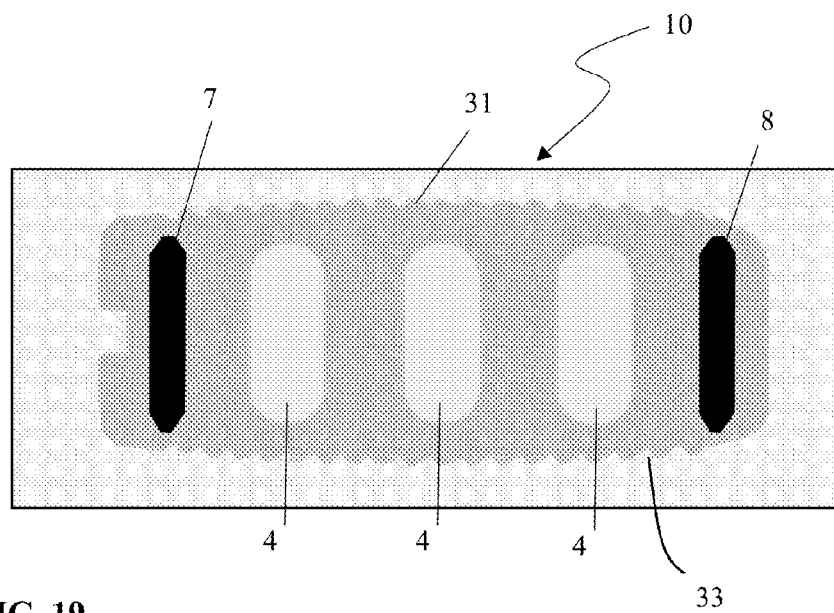


FIG. 19

FIG. 20

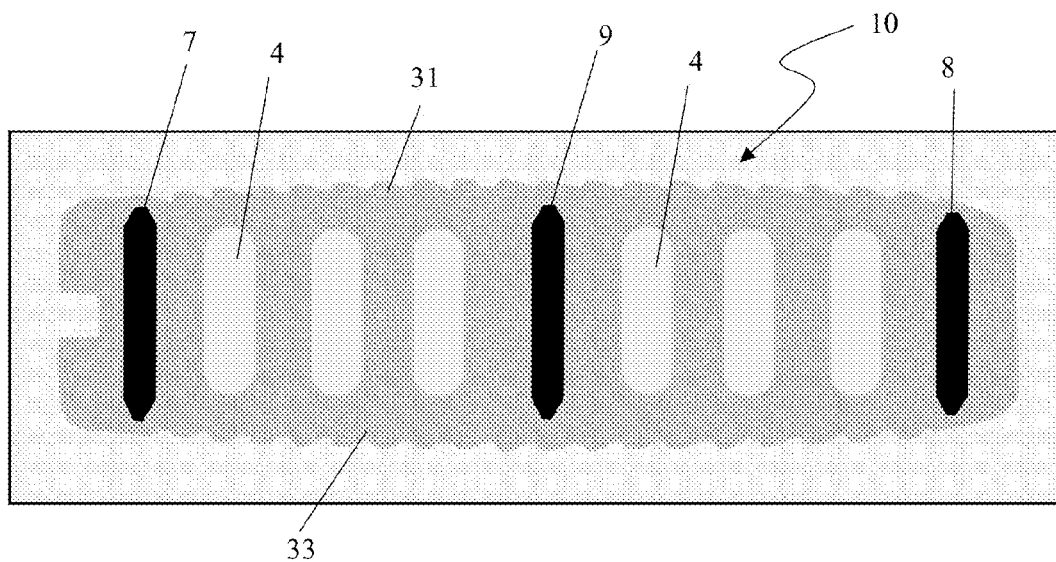
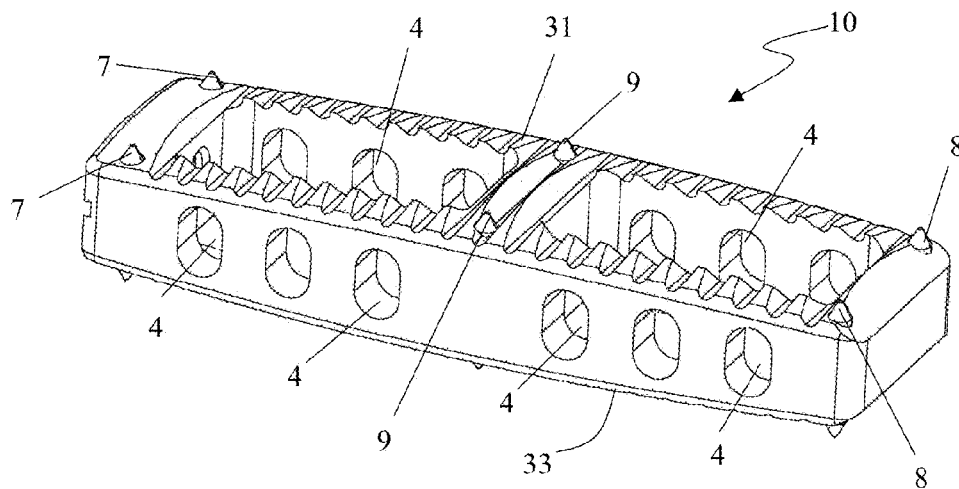


FIG. 21

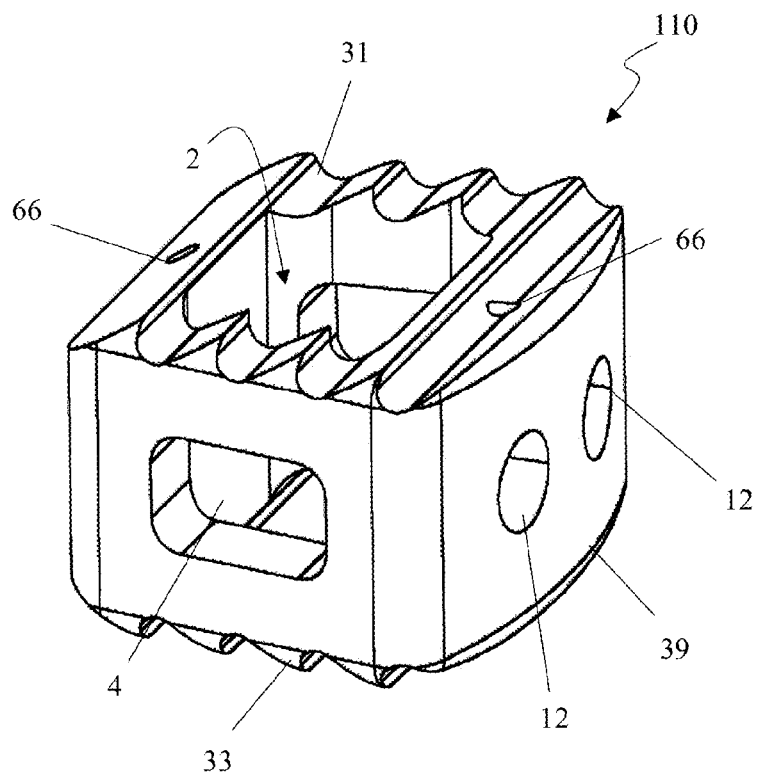


FIG. 22

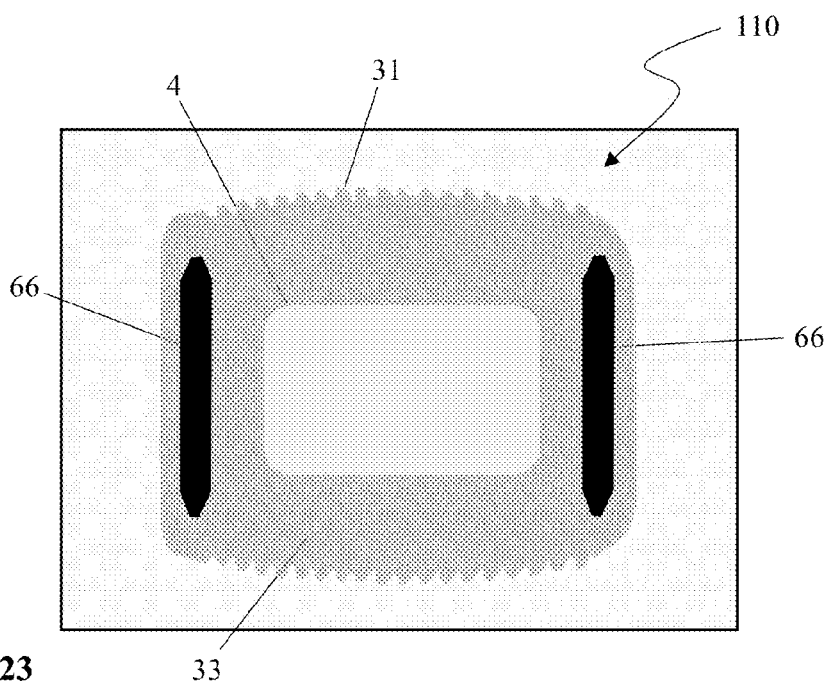


FIG. 23

SYSTEMS AND METHODS FOR SPINAL FUSION

CROSS-REFERENCE TO RELATED APPLICATIONS

This application is a continuation of U.S. patent application Ser. No. 14/171,484 filed Feb. 3, 2014, which is a continuation of U.S. patent application Ser. No. 14/066,285 filed Oct. 29, 2013 (now U.S. Pat. No. 8,685,105), which is a continuation of U.S. patent application Ser. No. 13/748,925 filed Jan. 24, 2013 (now U.S. Pat. No. 8,574,301), which is a continuation of U.S. patent application Ser. No. 13/747,765 filed Jan. 23, 2013 (now U.S. Pat. No. 8,608,804), which is a continuation of U.S. patent application Ser. No. 13/441,092 filed Apr. 6, 2012 (now U.S. Pat. No. 8,361,156), which is a continuation of U.S. patent application Ser. No. 13/440,062 filed Apr. 5, 2012 (now U.S. Pat. No. 8,246,686), which is a continuation of U.S. patent application Ser. No. 13/079,645 filed Apr. 4, 2011 (now U.S. Pat. No. 8,187,334), which is a continuation of U.S. patent application Ser. No. 11/093,409 filed Mar. 29, 2005 (now U.S. Pat. No. 7,918,891), which claims the benefit of the filing date under 35 USC 119(e) of United States Provisional Application entitled "Systems and Methods for Spinal Fusion," Ser. No. 60/557,536 filed Mar. 29, 2004, the entire contents of these prior applications are incorporated herein by reference.

BACKGROUND OF THE INVENTION

I. Field of the Invention

The present invention relates generally to spinal surgery and, more particularly, to a system and method for spinal fusion comprising a spinal fusion implant of non-bone construction releasably coupled to an insertion instrument dimensioned to introduce the spinal fusion implant into any of a variety of spinal target sites.

II. Discussion of the Prior Art

Currently there are nearly 500,000 spine lumbar and cervical fusion procedures performed each year in the United States. Such procedures are commonly performed to correct problems, such as chronic back or neck pain, which result from degenerated intervertebral discs or trauma. Generally, spinal fusion procedures involve removing some or all of the diseased or damaged disc, and inserting one or more intervertebral implants into the resulting disc space. Introducing the intervertebral implant serves to restore the height between adjacent vertebrae ("disc height"), which reduces if not eliminates neural impingement commonly associated with a damaged or diseased disc.

Autologous bone grafts are widely used intervertebral implant for lumbar fusion. Autologous bone grafts are obtained by harvesting a section of bone from the iliac crest of the patient and thereafter implanting the article of autologous bone graft to effect fusion. While generally effective, the use of autologous bone grafts suffers certain drawbacks. A primary drawback is the morbidity associated with harvesting the autologous graft from the patient's iliac crest. Another related drawback is the added surgical time required to perform the bone-harvesting.

Allograft bone grafts have been employed with increased regularity in an effort to overcome the drawbacks of autologous bone grafts. Allograft bone grafts are harvested from cadaveric specimens, machined, and sterilized for implantation. While allograft bone grafts eliminate the morbidity associated with iliac crest bone harvesting, as well as decrease the overall surgical time, they still suffer certain drawbacks. A

primary drawback is supply constraint, in that the tissue banks that process and produce allograft bone implants find it difficult to forecast allograft given the inherent challenges in forecasting the receipt of cadavers. Another related drawback is that it is difficult to manufacture the allograft with consistent shape and strength characteristics given the variation from cadaver to cadaver.

The present invention is directed at overcoming, or at least improving upon, the disadvantages of the prior art.

SUMMARY OF THE INVENTION

The present invention overcomes the drawbacks of the prior art by providing a spinal fusion system and related methods involving the use of a spinal fusion implant of non-bone construction. The non-bone construction of the spinal fusion implant of the present invention overcomes the drawbacks of the prior art in that it is not supply limited (as with allograft) and does not require harvesting bone from the patient (as with autograft). The spinal fusion implant of the present invention may be comprised of any suitable non-bone composition, including but not limited to polymer compositions (e.g. poly-ether-ether-ketone (PEEK) and/or poly-ether-ketone-ketone (PEKK)), ceramic, metal or any combination of these materials.

The spinal fusion implant of the present invention may be provided in any number of suitable shapes and sizes depending upon the particular surgical procedure or need. The spinal fusion implant of the present invention may be dimensioned for use in the cervical and/or lumbar spine without departing from the scope of the present invention. For lumbar fusion, the spinal fusion implant of the present invention may be dimensioned, by way of example only, having a width ranging between 9 and 18 mm, a height ranging between 8 and 16 mm, and a length ranging between 25 and 45 mm. For cervical fusion, the spinal fusion implant of the present invention may be dimensioned, by way of example only, having a width about 11 mm, a height ranging between 5 and 12 mm, and a length about 14 mm.

The spinal fusion implant of the present invention may be provided with any number of additional features for promoting fusion, such as apertures extending between the upper and lower vertebral bodies which allow a boney bridge to form through the spinal fusion implant of the present invention. Such fusion-promoting apertures may be dimensioned to receive any number of suitable osteoinductive agents, including but not limited to bone morphogenic protein (BMP) and bio-resorbable polymers, including but not limited to any of a variety of poly (D,L-lactide-co-glycolide) based polymers. The spinal fusion implant of the present invention is preferably equipped with one or more lateral openings which aid it provides in visualization at the time of implantation and at subsequent clinical evaluations.

The spinal fusion implant of the present invention may be provided with any number of suitable anti-migration features to prevent spinal fusion implant from migrating or moving from the disc space after implantation. Suitable anti-migration features may include, but are not necessarily limited to, angled teeth formed along the upper and/or lower surfaces of the spinal fusion implant and/or spike elements disposed partially within and partially outside the upper and/or lower surfaces of the spinal fusion implant. Such anti-migration features provide the additional benefit of increasing the overall surface area between the spinal fusion implant of the present invention and the adjacent vertebrae, which promotes overall bone fusion rates.

3

The spinal fusion implant of the present invention may be provided with any number of features for enhancing the visualization of the implant during and/or after implantation into a spinal target site. According to one aspect of the present invention, such visualization enhancement features may take the form of the spike elements used for anti-migration, which may be manufactured from any of a variety of suitable materials, including but not limited to a metal, ceramic, and/or polymer material, preferably having radiopaque characteristics. The spike elements may also take any of a variety of suitable shapes, including but not limited to a generally elongated element disposed within the implant such that the ends thereof extend generally perpendicularly from the upper and/or lower surfaces of the implant. The spike elements may each comprise a unitary element extending through upper and lower surfaces or, alternatively, each spike element may comprise a shorter element which only extends through a single surface (that is, does not extend through the entire height of the implant). In any event, when the spike elements are provided having radiodense characteristics and the implant is manufactured from a radiolucent material (such as, by way of example only, PEEK and/or PEKK), the spike elements will be readily observable under X-ray or fluoroscopy such that a surgeon may track the progress of the implant during implantation and/or the placement of the implant after implantation.

The spinal implant of the present invention may be introduced into a spinal target site through the use of any of a variety of suitable instruments having the capability to releasably engage the spinal implant. In a preferred embodiment, the insertion instrument permits quick, direct, accurate placement of the spinal implant of the present invention into the intervertebral space. According to one embodiment, the insertion instrument includes a threaded engagement element dimensioned to threadably engage into a receiving aperture formed in the spinal fusion implant of the present invention. According to another embodiment, the insertion instrument includes an elongate fork member and a generally tubular lock member.

BRIEF DESCRIPTION OF THE DRAWINGS

Many advantages of the present invention will be apparent to those skilled in the art with a reading of this specification in conjunction with the attached drawings, wherein like reference numerals are applied to like elements and wherein:

FIG. 1 is a perspective view of a spinal fusion system of the present invention, including a lumbar fusion implant releasably coupled to an insertion instrument according to one embodiment of the present invention;

FIG. 2 is a perspective view of the lumbar fusion implant of FIG. 1, illustrating (among other things) fusion apertures extending between top and bottom surfaces, a plurality of visualization apertures extending through the side walls, and a variety of anti-migration features according to one embodiment of the present invention;

FIG. 3 is a top view of the lumbar fusion implant of FIG. 1, illustrating (among other things) the fusion apertures and the anti-migration features according to one embodiment of the present invention;

FIG. 4 is a side view of the lumbar fusion implant of FIG. 1, illustrating (among other things) the visualization apertures, the anti-migration feature, and a receiving aperture for releasably engaging the insertion instrument of FIG. 1 according to one embodiment of the present invention;

FIG. 5 is an end view of the lumbar fusion implant of FIG. 1, illustrating (among other things) the receiving aperture

4

formed in the proximal end, the anti-migration features, and the visualization apertures according to one embodiment of the present invention;

FIG. 6 is an enlarged side view of the lumbar fusion implant of FIG. 1 releasably coupled to the distal end of the insertion instrument of FIG. 1 according to one embodiment of the present invention;

FIG. 7 is a perspective view of the insertion instrument of FIG. 1 in a fully assembled form according to one embodiment of the present invention;

FIG. 8 is an enlarged perspective view of the distal region of the insertion instrument of FIG. 1 according to one embodiment of the present invention;

FIG. 9 is a perspective exploded view of the insertion instrument of FIG. 1, illustrating the component parts of the insertion instrument according to one embodiment of the present invention;

FIG. 10 is a perspective view of a spinal fusion system of the present invention, including a cervical fusion implant releasably coupled to a cervical insertion instrument according to one embodiment of the present invention;

FIG. 11 is a perspective view of the proximal side of the cervical fusion implant of FIG. 10, illustrating (among other things) fusion apertures extending between top and bottom surfaces, a plurality of visualization apertures extending through the lateral walls, a plurality of receiving apertures, and a variety of anti-migration features according to one embodiment of the present invention;

FIG. 12 is a perspective view of the distal side cervical fusion implant of FIG. 10, illustrating (among other things) the visualization apertures and anti-migration features;

FIG. 13 is a top view of the cervical fusion implant of FIG. 10, illustrating (among other things) the fusion apertures and anti-migration features according to one embodiment of the present invention;

FIG. 14 is a side view of the cervical fusion implant of FIG. 10, illustrating (among other things) the visualization apertures, the anti-migration features, and one of two receiving apertures provided in the proximal end for releasably engaging the cervical insertion instrument of FIG. 10 according to one embodiment of the present invention;

FIG. 15 is a perspective view of the cervical fusion implant of the present invention just prior to attachment to the cervical insertion device according to one embodiment of the present invention;

FIG. 16 is a perspective view of the insertion instrument of FIG. 10 in a fully assembled form according to one embodiment of the present invention;

FIG. 17 is a perspective exploded view of the insertion instrument of FIG. 10, illustrating the component parts of the insertion instrument according to one embodiment of the present invention;

FIGS. 18 and 19 are perspective and side views, respectively, illustrating the "enhanced visualization" feature of the present invention as employed within a lumbar fusion implant according to one embodiment of the present invention;

FIGS. 20 and 21 are perspective and side views, respectively, illustrating the "enhanced visualization" feature of the present invention as employed within a lumbar fusion implant according to one embodiment of the present invention; and

FIGS. 22 and 23 are perspective and side views, respectively, illustrating the "enhanced visualization" feature of the present invention as employed within a cervical fusion implant according to one embodiment of the present invention.

DESCRIPTION OF THE PREFERRED EMBODIMENTS

Illustrative embodiments of the invention are described below. In the interest of clarity, not all features of an actual implementation are described in this specification. It will of course be appreciated that in the development of any such actual embodiment, numerous implementation-specific decisions must be made to achieve the developers' specific goals, such as compliance with system-related and business-related constraints, which will vary from one implementation to another. Moreover, it will be appreciated that such a development effort might be complex and time-consuming, but would nevertheless be a routine undertaking for those of ordinary skill in the art having the benefit of this disclosure. The system to facilitate bone fusion and related methods disclosed herein boasts a variety of inventive features and components that warrant patent protection, both individually and in combination.

FIG. 1 illustrates, by way of example only, a spinal fusion system 5 for performing spinal fusion between adjacent lumbar vertebrae, including an exemplary spinal fusion implant 10 and an exemplary insertion instrument 20 provided in accordance with the present invention. The spinal fusion implant 10 may be comprised of any suitable non-bone composition having suitable radiolucent characteristics, including but not limited to polymer compositions (e.g. poly-ether-ether-ketone (PEEK) and/or poly-ether-ketone-ketone (PEKK)) or any combination of PEEK and PEKK. The spinal fusion implant 10 of the present invention may be dimensioned, by way of example only, having a width ranging between 9 and 18 mm, a height ranging between 8 and 16 mm, and a length ranging between 25 and 45 mm.

As will be described in detail below, the insertion instrument 20 is configured to releasably maintain the exemplary spinal fusion implant 10 in the proper orientation during insertion into a lumbar disc space and thereafter release to deposit the implant 10. The exemplary spinal fusion implant 10, having been deposited in the disc space, facilitates spinal fusion over time by maintaining a restored disc height as natural bone growth occurs through and/or past the implant 10, resulting in the formation of a boney bridge extending between the adjacent vertebral bodies. The implant 10 is particularly suited for introduction into the disc space via a lateral (trans-psoas) approach to the spine, but may be introduced in any of a variety of approaches, such as posterior, anterior, antero-lateral, and postero-lateral, without departing from the scope of the present invention (depending upon the sizing of the implant 10).

The spinal fusion implant 10 of the present invention may be provided with any number of additional features for promoting fusion, such as apertures 2 extending between the upper and lower vertebral bodies which allow a boney bridge to form through the spinal fusion implant 10. According to a still further aspect of the present invention, this fusion may be facilitated or augmented by introducing or positioning various osteoinductive materials within the apertures 2 and/or adjacent to the spinal fusion implant 10. Such osteoinductive materials may be introduced before, during, or after the insertion of the exemplary spinal fusion implant 10, and may include (but are not necessarily limited to) autologous bone harvested from the patient receiving the spinal fusion implant 10, bone allograft, bone xenograft, any number of non-bone implants (e.g. ceramic, metallic, polymer), bone morphogenic protein, and bio-resorbable compositions, including but not limited to any of a variety of poly (D,L-lactide-co-glycolide) based polymers.

The spinal fusion implant 10 of the present invention is preferably equipped with one or more visualization apertures 4 situated along the lateral sides, which aid in visualization at the time of implantation and at subsequent clinical evaluations. More specifically, based on the generally radiolucent nature of the implant 10, the visualization apertures 4 provide the ability to visualize the interior of the implant 10 during X-ray and/or other suitable imaging techniques which are undertaken from the side (or "lateral") perspective of the implant 10. If fusion has taken place, the visualization apertures 4 will provide a method for the surgeon to make follow up assessments as to the degree of fusion without any visual interference from the spinal fusion implant 10. Further, the visualization apertures 4 will provide an avenue for cellular migration to the exterior of the spinal fusion implant 10. Thus the spinal fusion implant 10 will serve as additional scaffolding for bone fusion on the exterior of the spinal fusion implant 10.

FIGS. 2-5 depict various embodiments of the exemplary spinal fusion implant 10. Some common attributes are shared among the various embodiments. More specifically, each spinal fusion implant 10 has a top surface 31, a bottom surface 33, lateral sides 14, a proximal side 22, and a distal side 16. In one embodiment, the top and bottom surfaces 31, 33 are generally parallel. It can be appreciated by one skilled in the art that although the surfaces 31, 33 are generally parallel to one another, they may be provided in any number of suitable shapes, including but not limited to concave and/or convex. When provided as convex shapes, the top and bottom surfaces 31, 33 may better match the natural contours of the vertebral end plates. Although not shown, it will be appreciated that the top and bottom surfaces 31, 33 may be angled relative to one another to better match the natural lordosis of the lumbar and cervical spine or the natural kyphosis of the thoracic spine.

The exemplary spinal fusion implant 10 also preferably includes anti-migration features designed to increase the friction between the spinal fusion implant 10 and the adjacent contacting surfaces of the vertebral bodies so as to prohibit migration of the spinal fusion implant 10 after implantation. Such anti-migration features may include ridges 6 provided along the top surface 31 and/or bottom surface 33. Additional anti-migration features may also include a pair of spike elements 7 disposed within the proximal region of the implant 10, a pair of spike elements 8 disposed within the distal region of the implant 10, and a pair of spike elements 9 disposed within the central region of the implant 10. Spike elements 7, 8, 9 may extend from the top surface 31 and/or bottom surface 33 within the respective proximal, distal and central regions of the implant 10. The spike elements 7, 8, 9 may be manufactured from any of a variety of suitable materials, including but not limited to a metal, ceramic, and/or polymer material, preferably having radiopaque characteristics. The spike elements 7, 8, 9 may also take any of a variety of suitable shapes, including but not limited to a generally elongated element disposed within the implant 10 such that the ends thereof extend generally perpendicularly from the upper and/or lower surfaces 31, 33 of the implant 10. As best appreciated in FIG. 4, the spike elements 7, 8, 9 may each comprise a unitary element extending through upper and lower surfaces 31, 33. Alternatively, each spike element 7, 8, 9 may comprise a shorter element which only extends through a single surface 31, 33 (that is, does not extend through the entire height of the implant 10). In any event, when the spike elements 7, 8, 9 are provided having radiodense characteristics and the implant 10 is manufactured from a radiolucent material (such as, by way of example only, PEEK and/or PEKK), the spike elements 7, 8, 9 will be readily observable under X-ray or fluoro-

roscopy such that a surgeon may track the progress of the implant 10 during implantation and/or the placement of the implant 10 after implantation.

The spinal fusion implant 10 has two large fusion apertures 2, separated by a medial support 50, extending in a vertical fashion through the top surface 31 and bottom surface 33. The fusion apertures 2 function primarily as an avenue for bony fusion between adjacent vertebrae. The fusion apertures 2 may be provided in any of a variety of suitable shapes, including but not limited to the generally rectangular shape best viewed in FIG. 3, or a generally circular, oblong and/or triangular shape or any combination thereof. The spinal fusion implant 10 may have a plurality of visualization apertures 4 which allow a clinician to make visual observations of the degree of bony fusion un-obscured by the lateral side 14 to facilitate further diagnosis and treatment. The visualization apertures 4 may be provided in any of a variety of suitable shapes, including but not limited to the generally oblong shape best viewed in FIG. 4, or a generally circular, rectangular and/or triangular shape or any combination thereof.

The spinal fusion implant 10 may be provided with any number of suitable features for engaging the insertion instrument 20 without departing from the scope of the present invention. As best viewed in FIGS. 4-6, one engagement mechanism involves providing a threaded receiving aperture 12 in the proximal sidewall 22 of the spinal fusion implant 10 of the present invention. The threaded receiving aperture 12 is dimensioned to threadably receive a threaded connector 24 on the insertion instrument 20 (as will be described in greater detail below). The receiving aperture 12 extends inwardly from the proximal side 22 in a generally perpendicular fashion relative to the proximal side 22. Although shown as having a generally circular cross-section, it will be appreciated that the receiving aperture 12 may be provided having any number of suitable shapes or cross-sections, including but not limited to rectangular or triangular. In addition to the receiving aperture 12, the spinal fusion implant 10 is preferably equipped with a pair of grooved purchase regions 60, 61 extending generally horizontally from either side of the receiving aperture 12. The grooved purchase regions 60, 61 are dimensioned to receive corresponding distal head ridges 62, 63 on the insertion instrument 20 (as will be described in greater detail below), which collectively provide an enhanced engagement between the implant 10 and instrument 20.

FIGS. 6-9 detail the exemplary insertion instrument 20 according to one embodiment of the invention. The exemplary insertion instrument 20 includes an elongate tubular element 28 and an inserter shaft 44. The elongate tubular element 28 is constructed with a distal head 26 at its distal end, distal head ridges 62, 63 on the distal end of the distal head 26, a thumbwheel housing 38 at its proximal end and a handle 42 at its proximal end. The elongate tubular element 28 is generally cylindrical and of a length sufficient to allow the device to span from the surgical target site to a location sufficiently outside the patient's body so the handle 42 and thumbwheel housing 38 can be easily accessed by a clinician or a complimentary controlling device.

The elongate tubular element 28 is dimensioned to receive a spring 46 and the proximal end of the inserter shaft 44 into the inner bore 64 of the elongate tubular element 28. The inserter shaft 44 is dimensioned such that the threaded connector 24 at the distal end of the inserter shaft 44 just protrudes past the distal head ridges 62, 63 to allow engagement with the receiving aperture 12 of the spinal fusion implant 10. It should be appreciated by one skilled in the art that such a construction allows the inserter shaft 44 to be able to rotate

freely within the elongate tubular element 28 while stabilized by a spring 46 to reduce any slidable play in the insertion instrument 20.

The handle 42 is generally disposed at the proximal end of the insertion instrument 20. The handle 42 is fixed to the thumbwheel housing 38 allowing easy handling by the clinician. Because the handle 42 is fixed the clinician has easy access to the thumbwheel 34 and can stably turn the thumbwheel 34 relative to the thumbwheel housing 38. Additionally, the relative orientation of the thumbwheel housing 38 to the handle 42 orients the clinician with respect to the distal head 26 and distal head ridge 62. By way of example, the thumbwheel housing 38 holds a thumbwheel 34, a set screw 32, and a spacer 36. The inserter shaft 44 is attached to the thumbwheel 34 and is freely rotatable with low friction due to the spacer 36. One skilled in the art can appreciate myriad methods of assembling a housing similar to the above described.

FIG. 6 details the distal head ridge of the exemplary insertion instrument 20 coupled to the spinal fusion implant 10 through the purchase regions 60, 61. The distal head ridges 62, 63 are dimensioned to fit slidably into the purchase regions 60, 61 with low friction to allow accurate engagement of the threaded connector 24 to the receiving aperture 12 of the spinal fusion implant 10. In the presented embodiment, the outer dimension of the threaded connector 24 is smaller than the largest outer dimension of the distal head 26 and elongate tubular element 28. Alternatively, other methods of creating a gripping surface are contemplated including but not limited to knurling or facets.

In order to use the system to perform a spinal fusion procedure, the clinician must first designate the appropriate implant size. After the spinal fusion implant 10 is chosen, the distal head ridges 62, 63 of the inserter shaft 44 are inserted into the purchase regions 60, 61 of the spinal fusion implant 10. At that time the spinal fusion implant 10 and insertion instrument 20 are slidably engaged with one another. Before the clinician can manipulate the combined spinal fusion implant 10 and insertion instrument 20, they must be releasably secured together. In order to secure the spinal fusion implant 10 onto the threaded connector 24 of the inserter instrument 20, the clinician employs the thumbwheel 34 to rotate the inserter shaft 44 and threaded connector 24. The rotation of the threaded connector 24 will releasably engage the receiving aperture of the spinal fusion implant 10 and stabilize the insertion instrument 20 relative to the spinal fusion implant 10.

A clinician can utilize the secured system in either an open or minimally invasive spinal fusion procedure. In either type of procedure, a working channel is created in a patient that reaches the targeted spinal level. After the creation of that channel, the intervertebral space may be prepared via any number of well known preparation tools, including but not limited to Kerrisons, rongeurs, pituitaries, and rasps. After preparation, the insertion instrument 20 is used to place a spinal fusion implant 10 into the prepared intervertebral space. Once the implant 10 is inserted into the prepared space, the implant 10 is released from the insertion instrument 20 by rotating the thumbwheel 34 to disengage the threaded connector 24 from the receiving aperture 12. That motion removes the compressive force on the purchase regions 60, 61 between the distal head 26 and the distal head ridges 62, 63 of the spinal fusion implant 10 and allows the insertion instrument to be slidably removed from the implant 10. After the threaded connector 24 is disengaged from the implant 10, the insertion instrument 20 is removed from the working channel and the channel is closed. As previously mentioned, addi-

tional materials may be included in the procedure before, during or after the insertion of the spinal fusion implant **10** to aid the natural fusion of the targeted spinal level.

FIG. **10** illustrates a spinal fusion system **105** for performing spinal fusion between adjacent cervical vertebrae, including an exemplary spinal fusion implant **110** and an exemplary cervical insertion instrument **120** provided in accordance with the present invention. The spinal fusion implant **110** may comprise of any suitable non-bone composition having suitable radiolucent characteristics, including but not limited to polymer compositions (e.g. poly-ether-ether-ketone (PEEK) and/or poly-ether-ketone-ketone (PEKK)) or any combination of PEEK and PEKK. The spinal fusion implant **110** may be provided in any number of suitable sizes, such as, by way of example only, a width ranging between 11 to 14 mm, a height ranging between 5 and 12 mm, and a length ranging from 14 and 16 mm.

As will be described in detail below, the cervical insertion instrument **120** is configured to releasably maintain the exemplary cervical fusion implant **110** in the proper orientation for insertion. The cervical fusion implant **110** may be simultaneously introduced into a disc space while locked within the cervical insertion instrument **120** and thereafter released. The exemplary cervical fusion implant **110**, having been deposited in the disc space, effects spinal fusion over time as the natural bone healing process integrates and binds the implant with the adjacent vertebral bodies. This fusion may be facilitated or augmented by introducing or positioning various materials in a space created within or adjacent to the cervical fusion implant **110**. Those materials may be introduced before, during, or after the insertion of the exemplary cervical fusion implant **110**. The additional material may include bone autograft harvested from the patient receiving the spinal fusion implant **10**, one or more additional bone allograft, bio-resorbables or xenograft implants, any number of non-bone implants, and any number of fusion promoting compounds such as bone morphogenic protein.

FIGS. **11-14** depict various embodiments of the exemplary cervical fusion implant **110**. Some common attributes are shared among the various embodiments. More specifically, each cervical fusion implant **110** has a top surface **31**, a bottom surface **33**, lateral sides **14**, a proximal side **22**, and a distal side **16**. In one embodiment, the top and bottom surfaces **31**, **33** are generally parallel. It can be appreciated by one skilled in the art that although the surfaces are generally parallel, that the top **31** and bottom **33** surfaces may be angled with respect to one another to match the natural curve of the spine (i.e. lordosis or kyphosis). By way of example, implants for the cervical or lumbar regions of the spine will have anterior height greater than the posterior height to match the natural lordosis in those regions. Inversely, the implants designed for implantation into the thoracic region will be manufactured with a posterior height greater than the anterior height to match the natural kyphosis in that region. Additionally, the angled surface can aid in overall fit within the vertebral disc space.

The cervical fusion implant **110** preferably includes two receiving apertures **12** which are centrally aligned on the proximal side **22**. The receiving apertures **12** extend inwardly from the proximal side **22** in a generally perpendicular fashion relative to the proximal side **22**. Although shown as having a generally circular cross-section, it will be appreciated that the receiving aperture **12** may be provided having any number of suitable shapes or cross-sections, including but not limited to rectangular or triangular.

The exemplary cervical fusion implant **110** also preferably includes anti-migration features such as anti-migration teeth

6 along the top surface **31** and bottom surface **33**. Additional anti-migration features may include a plurality of proximal anti-migration spikes **68** and/or distal anti-migration spikes **70** integrated vertically through the cervical fusion implant **110**. The anti-migration features increase the friction between the cervical fusion implant **110** and the adjacent contacting surfaces of the vertebral bodies. That friction prohibits migration of the cervical fusion implant **110** during the propagation of natural bony fusion. It should be appreciated by one skilled in the art that such anti-migration teeth **6** can be oriented in a any manner other than generally vertically (as shown) without departing from the scope of the present invention. Moreover, as described above, the spikes **68**, **70** may be constructed from any of a variety of radiopaque materials, including but not limited to a metal, ceramic, and/or polymer material. When the spike elements **68**, **70** are provided having such radiodense characteristics, and the implant **110** is manufactured from a radiolucent material (such as, by way of example only, PEEK and/or PEKK), the spike elements **68**, **70** will be readily observable under X-ray or fluoroscopy such that a surgeon may track the progress of the implant **110** during implantation and/or the placement of the implant **110** after implantation.

The cervical fusion implant **110** has one large fusion aperture **2**, extending in a vertical fashion through the top surface **31** and bottom surface **33** which will function primarily as the avenue for bony fusion between adjacent vertebrae. The cervical fusion implant **110** may have a plurality of visualization apertures **4** which can also serve as an avenue of bony fusion on the lateral sides **14** via cell migration or additional adjuvants. The visualization apertures **4** serve an additional function of allowing a clinician to make visual observations of the degree of bony fusion un-obscured by the lateral side **14** to facilitate further diagnosis and treatment.

FIG. **15** illustrates, by way of example, the orientation of the cervical fusion implant **110** prior to attachment to the cervical insertion instrument **120** by a clinician. One skilled in the art would appreciate that although the current embodiment shows a slidable engagement, various other methods of engagement are contemplated, such as, threadable or hooking features.

FIGS. **16-17** detail the tubular lock member **21** of the exemplary cervical inserter instrument **110**. The tubular lock member **21** includes a central bore **25** dimensioned to receive the proximal end of the elongate fork member **11** therein. The internal dimension of the central bore **25** is smaller than the largest freestanding outer dimension of the taper feature **19**. As a result, the portion of the elongate fork member **11** that may be received by the central bore **25** of the tubular lock member **21** is limited by interference between the distal end of the tubular lock member **21** and the taper feature **19** of the elongate fork member **11**. In the present embodiment, the outer dimension of the threaded feature **13** of the elongate fork member **11** is smaller than the largest outer dimension of the taper feature **19** on the elongate fork member **11**. A thread feature **23** (not shown) at the proximal end of the tubular lock member **21** is situated inside the central bore **25**. The thread feature **23** matches the thread feature **13** on the elongate fork member **11** so that they can be threadably attached to one another. To ease the rotation of the tubular lock member **21** by hand, two semi-circular wings **27** may be provided protruding laterally outward from either side of the tubular lock member **21**. Alternatively, other methods of creating a gripping surface are contemplated including but not limited to knurling or facets.

A clinician can utilize the secured system in either an open or minimally invasive spinal fusion procedure. In either type

11

of procedure, a working channel is created in a patient that reaches the targeted spinal level. After the creation of that channel, the intervertebral space would be prepared (via known instruments as described above). After preparation, the insertion instrument 120 is used to place a cervical fusion implant 110 into the prepared intervertebral space. Once the cervical fusion implant 110 is inserted into the prepared space, the implant 110 is released from the cervical insertion instrument 120 by retracting the tubular lock member 21 from the elongate fork member 11 by rotating the tubular lock member 21 with respect to the elongate fork member 11 in the opposite direction from that used to initially secure the implant 110. That motion removes the compressive force on the purchase region 39 between the apertures 12 of the cervical fusion implant 110 and allows the engagement features 17 to be slidably removed from the apertures 12. After the engagement features 17 are disengaged from the cervical fusion implant 110, the cervical inserter instrument 120 is removed from the working channel and the channel is closed. As previously mentioned, additional materials may be included in the procedure before, during or after the insertion of the cervical fusion implant 110 to aid the natural fusion of the targeted spinal level.

In order to use the system to perform a spinal fusion procedure, the clinician must first designate the appropriate implant size. After the cervical fusion implant 110 is chosen, the engagement features 17 of the elongate fork member 11 are inserted into the apertures 12 on the implant 110. At that time the cervical fusion implant 110 and elongate fork member 11 are slidably engaged with one another. Before the clinician can manipulate the combined cervical fusion implant 110 and elongated fork member 11, they must be releasably secured together. In order to secure the cervical fusion implant 110 onto the elongate fork member 11, the clinician would next employ the tubular lock member 21. The clinician would insert the proximal end of the elongate fork member 11 into the central bore 25 of the tubular lock member 21 at its distal end. The tubular lock member 21 would then be advanced over the elongate fork member 11 until the thread feature 13 of that member and the thread feature 23 of the tubular lock member 21 become engaged.

Once engaged, advancement of the tubular lock member requires rotation of the tubular lock member 21 with respect to the elongate fork member 11. Preferably, after only a small amount of engagement of the thread features the distal end of the tubular lock member 21 would contact the taper feature 19 of the elongate fork member 11. The tubular lock member 21 would be advanced creating greater interference as the distal end approaches the distal end of the taper feature 19 which has the larger outer dimension. The increasing interference would laterally displace the clamping arms 15 of the elongate fork member 11 towards each other. Since the engagement features 17 of the elongate fork member 11 were initially inserted into the apertures 12 of the exemplary cervical fusion implant 110, the displacement of the clamping arms 15 would create a compressive force on the purchase region 39 separating the apertures 12 of the exemplary cervical fusion implant 110. That compressive force allows a clinician to manipulate the system without the exemplary cervical fusion implant 110 becoming disengaged from the cervical inserter instrument 120.

The enhanced visualization features of the implants 10, 110 are explained in greater detail with reference to FIGS. 18-23. FIG. 18 illustrates an implant 10 dimensioned particularly for use in a posterior approach (PLIF) having (by way of example only) a width ranging between 9 and 11 mm, a height ranging between 8 and 14 mm, and a length ranging between

12

25 and 30 mm. FIG. 19 illustrates the implant 10 of FIG. 18 from a side perspective via as taken via X-ray or fluoroscopy techniques, clearly showing the location of the spike elements 7 and 8 (there is no central spike element 9 as with FIG. 1) relative to the implant 10 and visualization apertures 4. FIG. 20 illustrates an implant 10 dimensioned particularly for use in a lateral approach (XLIF™ by NuVasive) having (by way of example only) a width of approximately 18 mm, a height ranging between 8 and 16 mm, and a length ranging between 40 and 45 mm. FIG. 21 illustrates the implant 10 of FIG. 20 from a side perspective via as taken via X-ray or fluoroscopy techniques, clearly showing the location of the spike elements 7, 8, 9 relative to the implant 10 and visualization apertures 4. FIG. 22 illustrates an implant 110 dimensioned particularly for use in the cervical spine having (by way of example only) a width of approximately 11 mm, a height ranging between 5 and 12 mm, and a length of approximately 14 mm. FIG. 23 illustrates the implant 110 of FIG. 22 from a side perspective via as taken via X-ray or fluoroscopy techniques, clearly showing the location of the spike elements 66 relative to the implant 110 and visualization apertures 4. In this fashion, a surgeon may easily track the progress of the implant 10, 110 during implantation and/or after implantation by visualizing the spike elements 7, 8, 9 and 66, respectively, under X-ray and/or fluoroscopy according to the present invention.

While the invention is susceptible to various modifications and alternative forms, specific embodiments thereof have been shown by way of example in the drawings and are herein described in detail. It should be understood, however, that the description herein of specific embodiments is not intended to limit the invention to the particular forms disclosed, but on the contrary, the invention is to cover all modifications, equivalents, and alternatives falling within the spirit and scope of the invention as defined by the appended claims.

For example, while described herein primarily with reference to the lumbar and cervical spinal surgery, it is to be readily appreciated that the spinal fusion implants of the present invention may be suitable for accomplishing fusion in the thoracic spine without departing from the scope of the present invention. Moreover, it is to be readily appreciated that the insertion tools described herein may be employed with implants of any number of suitable constructions, including but not limited to metal, ceramic, plastic or composite.

What is claimed is:

1. A spinal fusion implant positionable within an interbody space between a first vertebra and a second vertebra, said implant comprising:

an upper surface including anti-migration elements to contact said first vertebra when said implant is positioned within the interbody space, a lower surface including anti-migration elements to contact said second vertebra when said implant is positioned within the interbody space, a distal wall, a proximal wall, a first sidewall, and a second sidewall opposite from the first sidewall, wherein the first sidewall intersects the proximal wall and the distal wall, wherein the second sidewall intersects the proximal wall and the distal wall, wherein the implant defines a straight longitudinal axis extending between the proximal wall and the distal wall, wherein said distal wall, proximal wall, first sidewall, and second sidewall comprise a radiolucent material, wherein the proximal wall includes a tooling aperture axially aligned with the longitudinal axis for releasably mating with an inserter tool;

wherein said implant has a longitudinal length greater than 40 mm extending from a proximal end of said proximal

13

wall to a distal end of said distal wall and extending parallel to said longitudinal axis, wherein said implant has a maximum lateral width extending from the first sidewall to the second sidewall along a medial plane that is perpendicular to said longitudinal axis, said implant has a maximum height extending from said upper surface to said lower surface and extending perpendicular to said longitudinal length and said maximum lateral width, wherein said wherein the longitudinal length of the implant is at least two and half times greater than the maximum lateral width, and said maximum lateral width is greater than said maximum height;

at least a first fusion aperture defined by the implant and extending through the implant from said upper surface to said lower surface and configured to permit bone growth between the first vertebra and the second vertebra when said implant is positioned within the interbody space, said first fusion aperture having: a longitudinal aperture length extending parallel to the longitudinal length of said implant and parallel to the longitudinal axis, and a lateral aperture width extending between said first sidewall to said second sidewall, wherein the longitudinal aperture length is greater than the lateral aperture width, wherein opposing portions of the first and second sidewalls positioned laterally of the first fusion aperture include outwardly bowed regions that are outwardly bowed away from said longitudinal axis along a direction extending between the proximal wall and distal wall, wherein the outwardly bowed region of the first sidewall is symmetric with the outwardly bowed region of the second sidewall relative to said longitudinal axis; and

means for radiopaque marking said distal wall being positioned in the radiolucent material of said distal wall, means for radiopaque marking said proximal wall being positioned in the radiolucent material of said proximal wall, and a pair of means for radiopaque marking a location of said medial plane in which said maximum lateral width extends, said pair of radiopaque means extending in said medial plane and being positioned in the radiolucent material of said first and second sidewalls.

2. The spinal fusion implant of claim 1, wherein said anti-migration elements of the upper surface include parallel ridges that extend along the first and second sidewalls, wherein said anti-migration elements of lower surface include parallel ridges along the first and second sidewalls, and wherein the upper and lower surfaces along the proximal wall and the distal wall are free of parallel ridges.

3. The spinal fusion implant of claim 2, wherein said parallel ridges of said upper surface extend perpendicular to said longitudinal axis.

4. The spinal fusion implant of claim 3, wherein said parallel ridges of said lower surface extend perpendicular to said longitudinal axis.

5. The spinal fusion implant of claim 2, wherein two of said parallel ridges of said upper surface extend over a medial support wall extending between the first and second sidewalls, wherein said medial support wall is positioned along said medial plane.

6. The spinal fusion implant of claim 1, wherein said pair of means for radiopaque marking a location of said medial plane are symmetric to one another relative to a central longitudinal plane extending along the longitudinal axis.

7. The spinal fusion implant of claim 6, wherein said first sidewall is positioned symmetric with said second sidewall relative to the central longitudinal plane.

14

8. The spinal fusion implant of claim 7, wherein said first and second sidewalls each define at least one viewing aperture in communication with the first fusion aperture, wherein said at least one viewing aperture of the first sidewall is symmetric with said at least one viewing aperture of the second sidewall relative to the central longitudinal plane.

9. The spinal fusion implant of claim 1, wherein the implant comprises the first fusion aperture and a second fusion aperture.

10. The spinal fusion implant of claim 9, further comprising a medial support wall extending along said medial plane between the first and second sidewalls, wherein the first and second fusion apertures are positioned on opposite sides of a medial support wall.

11. The spinal fusion implant of claim 9, wherein the first fusion aperture is symmetric with the second fusion aperture relative to the medial plane.

12. The spinal fusion implant of claim 1, wherein said implant includes four openings defined in said second sidewall, a first pair of said four openings being located in the second sidewall on a first side of said medial plane, and a second pair of said four openings being located in the second sidewall on a second side of said medial plane.

13. The spinal fusion implant of claim 12, wherein the four openings defined in said second sidewall have the same shape.

14. The spinal fusion implant of claim 1, wherein said maximum lateral width of said implant is 18 mm.

15. The spinal fusion implant of claim 1, wherein the first fusion aperture is bisected by a central longitudinal plane extending along said longitudinal axis of the implant and parallel to said height of the implant.

16. The spinal fusion implant of claim 1, wherein said opposing portions of said first and second sidewalls are outwardly bowed away from one another such that said maximum lateral width of said implant is greater than a maximum lateral width of said distal wall and is greater than a maximum lateral width of said proximal wall.

17. The spinal fusion implant of claim 1, wherein said proximal wall includes first and second lateral grooves positioned laterally of said tooling aperture, and wherein said tooling aperture and said first and second lateral grooves are configured to releasably mate with a lateral, trans-psoas inserter tool.

18. The spinal fusion implant of claim 1, wherein said radiolucent material comprises PEEK.

19. The spinal fusion implant of claim 1, wherein said implant includes at least one visualization aperture extending through at least one of said first sidewall and said second sidewall.

20. The spinal fusion implant of claim 1, wherein said upper and lower surfaces are parallel to one another.

21. The spinal fusion implant of claim 1, wherein said upper and lower surfaces are angled relative to one another to approximately correspond to lordosis of a lumbar spine when said implant is positioned within the interbody space.

22. The spinal fusion implant of claim 1, wherein said first fusion aperture is one of generally rectangular and generally oblong in shape.

23. The spinal fusion implant of claim 1, wherein the lateral aperture width of said first fusion aperture is more than two time greater than a lateral thickness of said first sidewall and is more than two time greater than a lateral thickness of said second sidewall.

24. The spinal fusion implant of claim 1, further comprising an osteoinductive material positioned with said first fusion aperture.

15

25. The spinal fusion implant of claim 1, wherein said pair of means for radiopaque marking a location of said medial plane includes: a first elongate and cylindrical body oriented parallel to said height of the implant and positioned in the first sidewall, and a second elongate and cylindrical body oriented parallel to said height of the implant and positioned in the second sidewall.

26. The spinal fusion implant of claim 1, wherein said means for radiopaque marking said distal wall includes an elongate and cylindrical body oriented parallel to said height of the implant.

27. The spinal fusion implant of claim 1, wherein said means for radiopaque marking said proximal wall includes an elongate and cylindrical body oriented parallel to said height of the implant.

28. The spinal fusion implant of claim 1, wherein said means for radiopaque marking said proximal wall is positioned symmetric with said means for radiopaque marking said distal wall relative to said medial plane.

29. The spinal fusion implant of claim 1, further comprising second means for radiopaque marking said distal wall being positioned in the radiolucent material of said distal wall.

30. The spinal fusion implant of claim 1, further comprising second means for radiopaque marking said proximal wall being positioned in the radiolucent material of said proximal wall.

31. The spinal fusion implant of claim 1, wherein said first and second sidewalls each define at least one viewing aperture in communication with the first fusion aperture wherein said at least one viewing aperture of the first sidewall is symmetric

16

with said at least one viewing aperture of the second sidewall relative to a central longitudinal plane extending along said longitudinal axis of the implant and parallel to said height of the implant.

32. The spinal fusion implant of claim 1, wherein the outwardly bowed regions of the first and second sidewalls extend from the proximal wall to the distal wall such that a convex curvature extends the full length of each of the first and second sidewalls.

33. The spinal fusion implant of claim 1, wherein said pair of means for radiopaque marking a location of said medial plane are positioned between parallel ridges along the first and second sidewalls.

34. The spinal fusion implant of claim 1, wherein said pair of means for radiopaque marking a location of said medial plane comprise rods that are symmetric in shape to one another.

35. The spinal fusion implant of claim 1, wherein said means for radiopaque marking said proximal wall and said means for radiopaque marking said distal wall comprise rods that are symmetric in shape to one another.

36. The spinal fusion implant of claim 1, wherein said height of said implant extends in said medial plane, and wherein said height of said implant is greater than a distal face height of said distal wall and is greater than a proximal face height of said proximal wall.

37. The spinal fusion implant of claim 36, wherein said proximal face height of said proximal wall is greater than said distal face height of said distal wall.

* * * * *